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Spectral-based thickness profiling of the corpus callosum enhances anomaly detection in fetal alcohol spectrum disorders

Spectral-based thickness profiling of the corpus callosum in fetal alcohol spectrum disorders

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Scope Statement

The diagnosis of fetal alcohol spectrum disorders (FASD) encompasses the pathological consequences of prenatal alcohol exposure. The main target of the teratogenic effects of ethanol is the brain, leading subjects with FASD to exhibit not only a smaller brain but also recurrent focal brain abnormalities such as the commonly reported abnormal corpus callosum (CC). We previously showed a narrowing of the CC for brain size, using manual measurement and its usefulness in diagnostic procedure. This study introduces a fast and normalization-free tool to characterize CC morphology by automatically measuring its length and thicknesses on anatomical brain MRI. We described the slimming of the posterior part of the CC, considering brain size, in a series of 89 subjects with FASD compared to 126 typically developing controls. In addition to providing a detailed description of callosal damage in FASD, our study provides a better understanding of the fetotoxic damage of ethanol, independent of the overall reduction in brain size. We are convinced that our innovative tool for describing CC anatomy, which could be used in other pathologies, and our description of brain abnormalities in FASD, the frequency of which is a public health issue, will be of particular interest to your readers.

Conflict of interest statement

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

CRediT Author Statement

David Germanaud: Conceptualization, Data curation, Funding acquisition, Methodology, Resources, Supervision, Validation, Writing - review & editing. Eliot Kerdreux: Validation, Writing - review & editing. Julien Lefèvre: Conceptualization, Methodology, Software, Supervision, Validation, Visualization, Writing - review & editing. Justine Fraize: Conceptualization, Formal Analysis, Investigation, Methodology, Resources, Software, Validation, Visualization, Writing - original draft, Writing - review & editing. Lucie Hertz-Pannier: Conceptualization, Funding acquisition, Supervision, Validation, Writing - review & editing. Monique Elmaleh-Bergès: Data curation, Resources, Writing - review & editing. Richard Delorme: Resources, Writing - review & editing. Yann Leprince: Methodology, Supervision, Validation, Visualization, Writing - review & editing.

Keywords

FASD, fetal alcohol spectrum disorder, FAS, fetal alcohol syndrome, FDR, false discovery rate, MRI, magnetic resonance imaging, NDD, neurodevelopmental disorders, NS-FASD, non-syndromic FASD Corpus callosum, fetal alcohol spectrum disorders, fetal alcohol syndrome, Spectral analysis, diagnostic imaging, scaling analysis

Abstract

Word count: 350

Fetal alcohol spectrum disorders (FASD) range from fetal alcohol syndrome (FAS) to non-syndromic forms (NS-FASD). The neuroanatomical consequences of prenatal alcohol exposure are mainly the reduction in brain size, but also focal abnormalities such as those of the corpus callosum (CC). We previously showed a narrowing of the CC for brain size, using manual measurement and its usefulness to improve diagnostic certainty. Our aim was to automate these measurements of the CC and identify more recurrent abnormalities in FAS subjects, independently of brain size reduction.

We developed a fast, automated, and normalization-free method based on spectral analysis to generate thicknesses of the CC continuously and at singular points (genu, body, isthmus, and splenium), and its length (LCC). We applied it on midsagittal section of the CC extracted from T1-anatomical brain MRI of 89 subjects with FASD (52 FAS, 37 NS-FASD) and 126 with typically development (6-20 y-o). After adjusting for batch effect, we compared the mean profiles and thicknesses of the singular points across the 3 groups. For each parameter, we established variations with age (growth charts) and brain size in the control group (scaling charts), then identified participants with abnormal measurements (<10th percentile).

We confirmed the slimming of the posterior half of the CC in both FASD groups, and of the genu section in the FAS group, compared to the control group. We found a significant group effect for the LCC, genu, median body, isthmus, and splenium thicknesses ($p < 0.05$). We described a body hump whose morphology did not differ between groups. According to the growth charts, there was an excess of FASD subjects with abnormal LCC and isthmus, and of FAS subjects with abnormal genu and splenium. According to the scaling charts, this excess remained only for LCC, isthmus and splenium, undersized for brain size.

We characterized size-independent anomalies of the posterior part of the CC in FASD, with an automated method, confirming and extending our previous study. Our new tool brings the use of a neuroanatomical criterion including CC damage closer to clinical practice. Our results suggest that an FAS signature identified in NS-FASD, could improve diagnosis specificity.

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Ethics statements

Studies involving animal subjects

Generated Statement: No animal studies are presented in this manuscript.

Studies involving human subjects

Generated Statement: The studies involving humans were approved by Paris-Saclay research ethics committee (CER-Paris-Saclay-2020-094). Controls' data were used within the framework of the ethical authorizations of the primary studies (Gene and autism, Inserm C07-33). . The studies were conducted in accordance with the local legislation and institutional requirements. The ethics committee/institutional review board waived the requirement of written informed consent for participation from the participants or the participants' legal guardians/next of kin because written informed consent from the FASD participants' legal guardian/next of kin was not required to participate in this study in accordance with the national legislation and the institutional requirements. Written informed consent from the control participants' legal guardian/next of kin was required to participate in the initial study in accordance with the national legislation and the institutional requirements..

Inclusion of identifiable human data

Generated Statement: No potentially identifiable images or data are presented in this study.

Data availability statement

Generated Statement: The data analyzed in this study is subject to the following licenses/restrictions: The datasets presented in this article are not readily available because the data that support the findings of this study are available on request from the corresponding author. The data are not publicly available due to privacy or ethical restrictions.. Requests to access these datasets should be directed to Justine Fraize, justine.fraize@inserm.fr.

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Abbreviations: FASD, fetal alcohol spectrum disorder; FAS, fetal alcohol syndrome; FDR, false discovery rate; MRI, magnetic resonance imaging; NDD, neurodevelopmental disorders; NS-FASD, non-syndromic FASD.

Keywords: Corpus callosum, fetal alcohol spectrum disorders, fetal alcohol syndrome, Spectral analysis, diagnostic imaging, scaling analysis.

33 **Abstract**

34 **Introduction**

35 Fetal alcohol spectrum disorders (FASD) range from fetal alcohol syndrome (FAS) to non-
36 syndromic forms (NS-FASD). The neuroanatomical consequences of prenatal alcohol exposure
37 are mainly the reduction in brain size, but also focal abnormalities such as those of the corpus
38 callosum (CC). We previously showed a narrowing of the CC for brain size, using manual
39 measurement and its usefulness to improve diagnostic certainty. Our aim was to automate
40 these measurements of the CC and identify more recurrent abnormalities in FAS subjects,
41 independently of brain size reduction.

42 **Methods**

43 We developed a fast, automated, and normalization-free method based on spectral analysis
44 to generate thicknesses of the CC continuously and at singular points (genu, body, isthmus,
45 and splenium), and its length (LCC). We applied it on midsagittal section of the CC extracted
46 from T1-anatomical brain MRI of 89 subjects with FASD (52 FAS, 37 NS-FASD) and 126 with
47 typically development (6-20 y-o). After adjusting for batch effect, we compared the mean
48 profiles and thicknesses of the singular points across the 3 groups. For each parameter, we
49 established variations with age (growth charts) and brain size in the control group (scaling
50 charts), then identified participants with abnormal measurements (<10th percentile).

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52 We confirmed the slimming of the posterior half of the CC in both FASD groups, and of the
53 genu section in the FAS group, compared to the control group. We found a significant group
54 effect for the LCC, genu, median body, isthmus, and splenium thicknesses ($p < 0.05$). We
55 described a body hump whose morphology did not differ between groups. According to the
56 growth charts, there was an excess of FASD subjects with abnormal LCC and isthmus, and of
57 FAS subjects with abnormal genu and splenium. According to the scaling charts, this excess
58 remained only for LCC, isthmus and splenium, undersized for brain size.

59 **Conclusion**

60 We characterized size-independent anomalies of the posterior part of the CC in FASD, with an
61 automated method, confirming and extending our previous study. Our new tool brings the
62 use of a neuroanatomical criterion including CC damage closer to clinical practice. Our results
63 suggest that an FAS signature identified in NS-FASD, could improve diagnosis specificity.

64 1 Introduction

65 The diagnosis of fetal alcohol spectrum disorders (FASD) encompasses the pathological
66 consequences of prenatal alcohol exposure, which range from fetal alcohol syndrome (FAS)
67 to non-syndromic, non-specific forms (NS-FASD) (Astley, 2004; Cook et al., 2016; Hoyme et al.,
68 2016). The diagnosis of fetal alcohol syndrome (FAS) is determined by a consensual set of
69 clinical features, which include facial dysmorphia, growth retardation, and microcephaly. On
70 the other hand, the diagnosis of non-syndromic fetal alcohol spectrum disorder (NS-FASD),
71 which associate neurodevelopmental disorders with prenatal alcohol exposure, remains
72 probabilistic. The main target of the teratogenic effects of ethanol is the brain, leading
73 individuals with FASD to exhibit not only a smaller brain but also recurrent focal brain
74 abnormalities that are detectable via magnetic resonance imaging (MRI).

75 One of the most commonly reported focal brain abnormalities is the corpus callosum. This
76 large bundle of white matter fibers composed of interhemispheric homotopic axonal
77 projections turns out to be a privileged indicator of the consequences of prenatal alcohol
78 exposure. The last four large radiological description studies reported thinning, hypoplasia,
79 complete or partial agenesis of the corpus callosum in series composed of children either
80 prenatally exposed or with a diagnosis of FASD (Autti-Rämö et al., 2002; Astley, 2004; Boronat
81 et al., 2017; Treit et al., 2020; Fraize et al., 2023c). The prevalence of corpus callosum
82 anomalies that are visible to the naked eye, although partly subjective, could approach 3 to
83 10% in the FASD population. Computational neuroimaging has sought to uncover more subtle
84 anomalies or more objective morphometric descriptions. Several studies conducted on
85 subjects with FASD have suggested that the midsagittal corpus callosum area (Riley et al.,
86 1995; Sowell et al., 2001; Astley et al., 2009; Dodge et al., 2009; Fraize et al., 2023c), thickness
87 (Yang et al., 2012a), and volume (Gautam et al., 2014; Biffen et al., 2020; Inkelis et al., 2020)
88 may be reduced compared to controls. These changes have also been correlated with the
89 amount of prenatal alcohol consumption (Biffen et al., 2017; Jacobson et al., 2017). In addition
90 to a global reduction in the size of the corpus callosum in FASD, the posterior region appears
91 to be more severely affected in size (Sowell et al., 2001; Dodge et al., 2009; Fraize et al., 2023a)
92 or in shape, resulting in a flattened or misshapen appearance (Sowell et al., 2001; Bookstein
93 et al., 2002). However, these results need to be qualified, because even within the same team,
94 they were not always confirmed. In the study by Yang et al., where three series from different
95 sites were pooled, the thinning on the posterior part initially described (Sowell et al., 2001)
96 was found to be significant in only one sub-group (Yang et al., 2012a). Despite these detailed
97 descriptions, no neuroanatomical criterion referring explicitly to specific anomalies of the
98 corpus callosum have been added to the diagnostic guidelines (Astley, 2004; Cook et al., 2016;
99 Hoyme et al., 2016). Yet, we recently reported the narrowing of the isthmus to be a recurrent
100 anomaly in FAS, using objective manual measurements of callosal thickness and normative
101 scaling analysis (Fraize et al., 2023c). We proposed to integrate it into an explicit compound
102 neuroanatomical marker in the diagnostic decision tree. The ultimate goal is for
103 neuroanatomy to contribute to clinical assessment, especially for subjects with non-
104 syndromic forms.

105 To our knowledge, there is no fully automated reference tool for the measurement of the
106 corpus callosum thickness, let alone automated analysis methods to tag and obtain individual
107 measurements for singular points. Semi-automated measurement tools currently exist. For
108 instance, Luders et al. proposed a technique beginning with manually delineating the corpus

109 callosum on the sagittal midsection manually (Luders et al., 2006a). The upper and lower
110 contours are then differentiated to compute the mean distance and generate the median line.
111 The thickness of the corpus callosum is subsequently derived from this median line and
112 compared at each interval. Following this pioneering study, the approach was implemented
113 in the analysis of correlation with gender, IQ, and attention (Luders et al., 2006b, 2009, 2014;
114 Westerhausen et al., 2011). Adamson et al. proposed another more automated method, albeit
115 still involving human intervention (Adamson et al., 2011). Firstly, the two extremities are
116 manually placed on the contour of the corpus callosum which is automatically generated.
117 These two points are then adjusted to maximize the length of the center line. Subsequently,
118 the center line is divided into 40 points. Finally, the thickness of the corpus callosum is
119 determined by using either the orthogonality to the center line or by applying the Laplace
120 equation. A fully automated method was proposed by Herron et al. based on a series of radial
121 lines emanating from a centroid and intersecting the corpus callosum that are verticalized to
122 unwrap the structure, define a median line and measure thickness (Herron et al., 2012; Li et
123 al., 2017). The process relies on spatial normalization, the measurements being obtained in
124 the *Montreal Neurological Institute* (MNI) space and transformed back to native anatomical
125 space by inverting the affine spatial normalization transformation.

126 Regardless of how the thickness profile was obtained in these different studies (Sowell et al.,
127 2001; Luders et al., 2009; Yang et al., 2012b; Danielsen et al., 2020), the subsequent analyses
128 and comparisons required normalization into a common space. This normalization step is
129 supported by a hypothesis, not always explicit, about how the callosal thickness varies as a
130 function of the reference, either the full brain or the corpus callosum itself. It is also difficult
131 to anticipate how these post-normalization analyses would accommodate incompleteness of
132 the structure, for instance posterior agenesis for the corpus callosum, in terms of distortions
133 or loss of signal, depending on the choice of normalization or template (Mangin et al., 2016).
134 Normalization-based procedures and the underlying hypotheses are legitimate, but
135 questionable when studying pathological populations with abnormally small brain or high risk
136 of dysgenesis of the studied structure, which is the case with FASD and corpus callosum. At
137 the very least, this encourages strategies of generation and analysis of the corpus callosum
138 thickness profile that minimize the need for spatial normalization, above all spatial averaging,
139 and enable explicit size effect models to be implemented. Indeed, the local size deficits must
140 be interpreted by taking global brain size into account (scaling analysis) with a model that
141 allows proportions to vary with brain size (allometric scaling). The relevance of the power law
142 to describe the phenomena associated with brain size variations is firmly established (Toro et
143 al., 2009; Germanaud et al., 2012; Liu et al., 2014; de Jong et al., 2017; Warling et al., 2021;
144 Fraize et al., 2023b).

145 In this study, we first introduce a new method that is fast and fully automated, based on a first
146 step of spectral analysis of the shape of the corpus callosum, which makes it possible to define
147 and measure a continuous thickness profile at the individual level. We then propose a
148 normalization-free strategy of analysis of this profile based on automatically defined local
149 singular extrema. Lastly, we apply this spectral-based thickness profiling to a series of subjects
150 with FASD and controls. We characterize brain size independent callosal anomalies in a fully
151 automated manner, that were compared with the ones previously manually characterized in
152 the same population (Fraize et al., 2023c).

153 2 Materiel and methods

154 **Participants**

155 Eighty-nine consecutive subjects with FASD, aged 6 to 20 years, were retrospectively
 156 included from a clinical series of patients attending the dedicated child neurology consultation
 157 for neurodevelopmental disorders at Robert-Debré University Hospital (RD) between 2014
 158 and 2020. FASD diagnosis was established on the basis of the guidelines of Astley (Astley,
 159 2004) and a full differential diagnosis work-up was completed, including a systematic brain
 160 MRI. Individuals prenatally exposed to another embryo-fetotoxic agent were not included.
 161 FASD subjects were split into two groups: the syndromic FAS (including partial FAS) and the
 162 non-syndromic ones (NS-FASD). This series and the precise diagnostic procedure have already
 163 been described in previous studies (Fraize et al., 2023b, 2023c). Clinical and radiological
 164 characteristics of the 52 FAS subjects (58.4%) and the 37 NS-FASD subjects (41.6%) are
 165 detailed in **Table 1**.

166 One hundred and twenty-six typically developing subjects, aged 6 to 20 years, with no
 167 report of PAE, developmental delay or family history of neurological or psychiatric condition
 168 (1st degree) were included for comparison. A subgroup of 40 subjects was matched with the
 169 FASD group for the acquisition site (MRI scanner and sequence) as part of a research program
 170 on autism in the RD Psychiatry Department. Other typically developing subjects were part of
 171 previously published studies (Germanaud et al., 2014; Bouyeure et al., 2018).

172 There were no significant differences in the control group compared to the FASD group
 173 for sex (50.8% vs. 58.4% of males respectively, $p=0.334$) and age at MRI (12.08 vs.11.32 years
 174 of age respectively, $p=0.116$).

	FAS n = 52	NS-FASD n = 37	FASD groups comparison p-value
Sociodemographic assessment			
Sex: male n (%)	27 (51.9)	25 (67.6)	0.209
Age at MRI, mean in years (SD)	10.93 (3.57)	11.88 (3.55)	0.219
Clinical assessment, n (%)			
(1) Prenatal alcohol exposure			
4.Confirmed, severe	21 (40.4)	16 (43.2)	0.959
3.Confirmed, moderate or unquantified	26 (50.0)	19 (51.1)	1.000
2.Not documented	5 (9.6)	2 (5.4)	0.748
1.No exposure	0 (0.0)	0 (0.0)	-
(2) FAS facial features			
4.Severe	31 (59.6)	2 (5.4)	<0.001
3.Moderate	21 (40.3)	1 (2.7)	<0.001
2.Mild	0 (0.0)	30 (81.1)	<0.001
1.None	0 (0.0)	4 (10.8)	0.057
(3) Growth deficiency			
4.Significant	19 (36.5)	3 (8.1)	0.005
3.Moderate	11 (21.2)	2 (5.4)	0.077
2.Mild	9 (17.3)	9 (24.3)	0.586
1.None	13 (25.0)	23 (62.2)	0.001
Brain anatomy			

(4) Structural central nervous system damage	40 (76.9)	19 (51.4)	0.022
Head circumference (smallest known)			
(4) $\leq - 2$ SD: microcephaly	34 (65.4)	13 (35.1)	0.009

175 **Table 1. Demographic, clinical, radiological data of FASD subjects.** FAS: fetal alcohol syndrome;
 176 FASD: fetal alcohol spectrum disorder; NS-FASD: non-syndromic fetal alcohol spectrum
 177 disorder; SD: standard deviation. *In bold, p-values <0.05.*

178 This study was conducted in accordance with the principles of the Declaration of
 179 Helsinki. Subjects' data were studied in accordance with French regulation (MR-004,
 180 declaration of conformity n°2059980v0), following approval by the Paris-Saclay research
 181 ethics committee (CER-Paris-Saclay-2020-094). Controls' data were used within the
 182 framework of the ethical authorizations of the primary studies (Gene and autism, Inserm C07-
 183 33, 08-029 and 11-008).

184 2.1 MRI data

185 For both FASD subjects and 40 site-matched controls, MRI acquisitions were
 186 performed in the Department of Pediatric Radiology of RD Hospital at 1.5T (Ingenia, Philips
 187 Healthcare, Amsterdam, the Netherlands) with a 3DT1 FFE-TFE sequence (1 mm isotropic; TR
 188 = 8.2ms; TE = 3.8ms; TI = 0.8s; Flip = 8°; SENSE = 2). Another group of 31 controls was acquired
 189 at the Frédéric Joliot Hospital (SHFJ, CEA-Saclay) at 1.5T (Signa, GE Healthcare, Milwaukee, US)
 190 with a 3DT1 GE FSPGR sequence (1x1x1.2 mm; TR = 9.9ms; TE = 2ms; TI = 0.6s; Flip = 10°) and
 191 a third one of 55 controls subjects on a 3T (Siemens Trio, Siemens Healthineers, Oxford, UK)
 192 at NeuroSpin (NS, CEA-Saclay) with a 3DT1 Siemens MPRAGE sequence (1mm isotropic;
 193 TR=2.3s; TE = 3ms; TI = 0.9s; Flip = 9°; GRAPPA 2). A visual quality check was systematically
 194 performed (JF, DG) to exclude images of insufficient quality.

195 2.2 MRI processing

196 2.2.1 Total brain volume

197 The total brain volume was obtained by *volBrain* (Manjón and Coupé, 2016), and was highly
 198 correlated ($R^2 = 75\%$) with the previously used proxy of brain size, that is, the axial reference
 199 brain surface (**Figure 1, sup. mat.**) (Fraize et al., 2023c).

200 2.2.2 Midsagittal section of the corpus callosum

201 The mask of the midsagittal section of the corpus callosum was obtained within the
 202 *Morphologist2015* framework of *BrainVisa* (<https://brainvisa.info/>) after oversampling of the
 203 T1-weighted images at 0.5 mm isotropic resolution. This section was localized in the
 204 interhemispheric plane by intersecting the white matter mask with the midsagittal plane in
 205 the Talairach space. The mask was checked systematically for any obvious segmentation error
 206 that could be manually corrected (**Table 1, sup. mat.**).

207 2.2.3 Spectral analysis of the shape using the Fiedler vector

208 From the mask of the midsagittal section of the corpus callosum, we built a 26-connectivity
 209 graph. To do so, we considered the 3D points from the one row of voxel of the mask and added

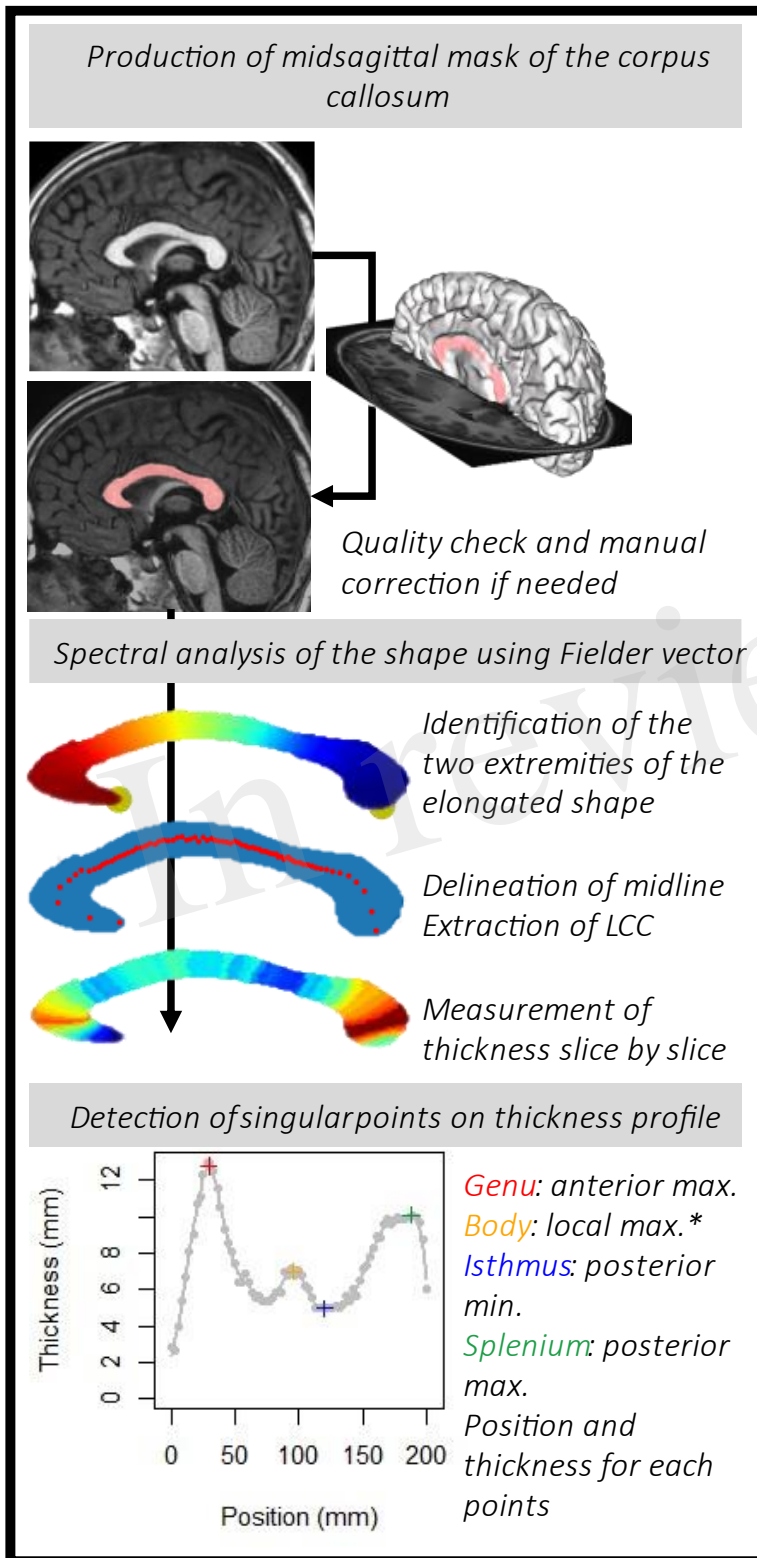
210 edges among the 26 possible neighbors if belongs to mask. We used the Fiedler vector of this
211 graph, the first non-trivial eigenvector of the Laplacian matrix, to compute a quasi-isometric
212 parameterization (Lefevre et al., 2012; Coulon et al., 2015). This mathematical tool tracked
213 the main elongation vector and identified extremal points. We added a simple algorithm to
214 reposition the rostrum so that its position is correct (see details in **sup. mat. Figure 2**). The
215 Laplacian graphs were perturbed to create a 'new' Fiedler vector that followed the correct
216 elongation (Lefèvre et al. 2023). From this 'new' Fiedler vector, we calculated isolines
217 (equivalent value). Then, regular bins were defined between the min and max values of the
218 Fiedler vector. It provided slices of the shape, of irregular width. The barycenter of each slice
219 was computed to form the midline (see the irregularly spaced red dots on the **Figure 1**). From
220 this midline and reparametrized vector, we obtained new isolines and slices of constant and
221 regular thickness. Using PCA within each slice, the main direction, roughly orthogonal to the
222 median line, was used to extract regular thicknesses. We finally obtained a map of the corpus
223 callosum thickness on regularly and optimally spaced slices (between 50 and 80) following the
224 longitudinal orientation of the shape. The code used to perform spectral analysis of the corpus
225 callosum midsagittal section is released on
226 <https://github.com/JulienLefevreMars/CorpusCallosumParameterization>.

227 *2.2.4 Thickness profile and singular points*

228 The first parameter of interest extracted was the length of the corpus callosum (LCC) obtained
229 from the length of the curvilinear abscissa between the two extreme points. Then, we targeted
230 the local singular extrema on the continuous thickness profile curve fitted with cubic
231 smoothing spline (smooth.spline() R function). The smoothing parameters were set at the
232 same level for each subject. *spar* is the smoothing parameter controlling the trade-off
233 between fidelity to the data and roughness of the function estimate. It is derived from the
234 lambda parameter, scaled between 0 and 1. Here, we fixed the *spar* parameter at 0.4. To
235 characterize the morphology of the corpus callosum, radiologists and clinicians usually
236 measure the thickness of the genu at the thickest point anteriorly, the body (local thickness),
237 the isthmus at the thinnest point posteriorly and the splenium at the thickest point
238 posteriorly)(Garel et al., 2011; Fraize et al., 2023c). From the thickness profiles, we extracted
239 the positions and the thicknesses of the genu (GT) and the splenium (ST), the local maximums
240 of the two extremities, and of the isthmus (IT), the local minimum between these two points.
241 In addition, we looked for localized thickening, a hump, within the body (**Figure 1**). As the
242 amplitude of this thickening could potentially be small and to make sure that it was
243 independent of curve smoothing variations, we sought it on the thickness profile curve
244 between the genu and the isthmus, by varying the level of smoothing (10 levels in addition to
245 the one initially chosen, from 0.2 to 0.7). To locate the body hump, we identified the local
246 maximum(s) whose position was consensual on the curvilinear abscissa on more than 8 of the
247 smoothing levels. We extracted the body hump thickness (BHT) or the mean thickness if there
248 were several humps (no more than two). We also extracted the median of the thicknesses
249 between the genu and the isthmus, as the median body thickness (MBT). All these processing
250 steps are summed up in **Figure 1**.

251 These length and thickness parameters were correlated with available gold standard manual
252 measures using the PACS measurement tools (Carestream, New York, NY, USA) (Fraize et al.,
253 2023c) by establishing the coefficient of determination R^2 and the mean percentage error

254 (MPE= mean of the difference between manual and automated measurements divided by
255 manual measurement).



256

257 **Figure 1. Pipeline to obtain the thickness profile for each subject and identify the points of**
258 **interest: the genu, the body hump (*see details in the text and in Figure 3), the isthmus and**
259 **the splenium.**

260 2.3 Modeling and statistical analysis

261 Statistics were performed using R Project for Statistical Computing (RRID:SCR_001905), with
262 a 5% alpha risk. A False Discovery Rate (FDR) method was systematically applied to correct for
263 multiple comparisons (Benjamini and Hochberg, 1995) at each analysis step (all parameters
264 together). Group differences in clinical characteristics and parameters were evaluated using
265 two-sample *t*-tests for continuous variables, and a Chi-square test for categorical variables,
266 ANOVA for group effect. To assess the normality assumption of the *t*-tests and the ANOVA,
267 we first performed the Kolmogorov-Smirnov test for each of the 3 groups, and the *p*-values
268 were not significant for any of the groups. A *p*-value is significant when the data do not appear
269 to be normally distributed.

270 Since the data were acquired on 3 sites, we adjusted for batch effect prior to analyses using
271 ComBat, a method based on an empirical Bayes framework (Johnson et al., 2007; Fortin et al.,
272 2018), integrating into the model sex, age, and diagnosis as covariates to be spared,
273 considering their possible interaction (**Table 3, sup. mat.**). We then performed unifactorial
274 group comparisons between FASD and controls knowing that these groups were matched for
275 age and sex. First we compared the whole thickness profile after rigid length normalization to
276 provide a continuous quantitative comparison of the radiological aspect of the corpus
277 callosum. Second, we compared the five parameters previously defined (callosal length and
278 the thickness of the 4 singular points). Lastly, we implemented clinically inspired normative
279 analysis to provide an individual-based comparison of these five parameters, accounting for
280 two major covariates i.e., age and brain size: first a normative growth analysis (age) then a
281 normative scaling analysis (brain size).

282 2.3.1 Unifactorial group comparison

283 We compared the thickness profiles of the controls with those of the two FASD groups. After
284 rigid spatial normalization in the curvilinear abscissa axis, we oversampled thicknesses along
285 this normed axis ($n = 100$) then adjusted for site effect. We studied the effect of FASD, using
286 a linear mixed model considering diagnosis (controls vs. FAS or NS-FASD) as a fixed effect and
287 random effect for each subject to account for subject-specific variability. Nonparametric
288 cluster-based permutation analyses were carried out using a method inspired by EEG-MEG
289 analysis to locate and group zones of significantly different thicknesses for spatial consistency
290 (originally, time-points with temporal consistency in EEG signals), considering corrections for
291 multiple comparisons (Maris and Oostenveld, 2007). Significance probability was calculated
292 using the cluster-mass statistic (cluster-forming $\alpha = 0.05$, randomizations = 1000).

293 2.3.2 Normative analyses

294 To define the growth curves, the relationships between measured parameters (LCC and
295 thicknesses at singular points adjusted for site effect) and age were modelled in the control
296 group. We applied a general additive model considering homoscedasticity over the age range
297 to fit the model and obtain percentiles of the distribution (Wood and Fasiolo, 2017; Dinga et
298 al., 2021).

299 To define the scaling curves, the relationships between measured parameters (*P*) and brain
300 size (total brain volume, TBV) were modelled in the control group, by a power law with scaling
301 coefficient *a* and constant *b* ($P = b \times TBV^a$) to take into account expected allometric effects

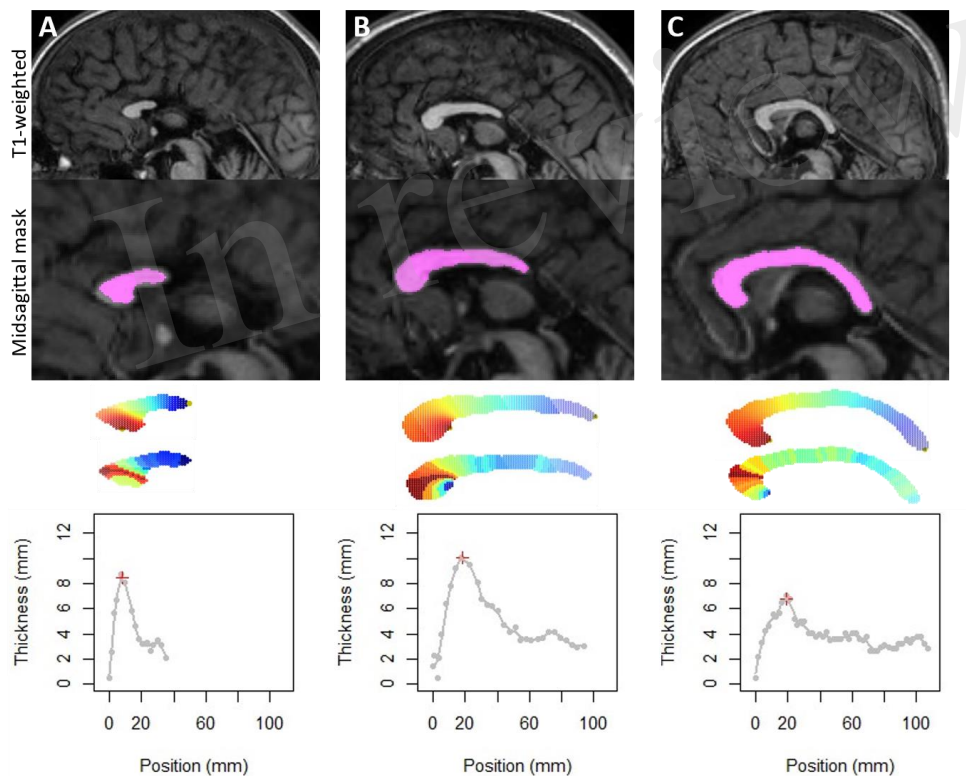
302 (changes in proportions with size) (Liu et al., 2014; de Jong et al., 2017; Warling et al., 2021).
303 Using bootstrap resampling and empirical quantiles, we obtained the unbiased prediction
304 intervals (90th and 10th percentiles) (Guenther, 1971; Lee and Scholtes, 2014).

305 For each parameter, FASD subjects with measurements below the 10th percentile curve were
306 counted as normatively too small for age or for brain size. An abnormality was considered
307 recurrent when the number of too-small measurements in the FAS or NS-FASD group
308 exceeded the theoretically expected 10% of the individuals (binomial test).

309 3 Results

310 3.1 Identification of singular points

311 The method was successfully applied to all subjects. For the two FAS subjects with posterior
312 agenesis and the one with an obvious posterior thinning, the thickness profile was also
313 extracted and analyzed (**Figure 2**). They were not included for further analysis as they were
314 obvious outliers with missing singular points.



315

316 **Figure 2. Application of the method on the three FAS subjects with partial agenesis (A, B) or**
317 **with too thin corpus callosum (C), which could also be considered as a very posterior**
318 **agenesis of the splenium.** Note that our method detects the longest elongation and allows us
319 to obtain thicknesses by slice. On the other hand, detection of singular points was not possible.

320 From the thickness profiles, we were able to identify for each subject the position and
321 thickness of the genu, isthmus and splenium automatically.

322 We divided the subjects into 4 types to define the presence or not of the body hump. In type
 323 1, the position of the body hump was obvious and consensual for all smoothing levels,
 324 accounting for 78 subjects (36.8%). In type 2, the position of the body hump was obvious and
 325 consensual for more than 8 smoothing levels, accounting for 70 subjects (33.0%). In type 3,
 326 two body humps were obvious and consensual for more than 8 smoothing levels, accounting
 327 for 30 subjects (14.2%). In type 4, no body hump was identified, accounting for 34 subjects
 328 (16.0%) (Figure 3).

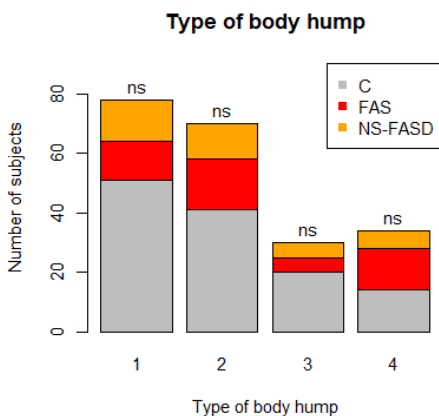
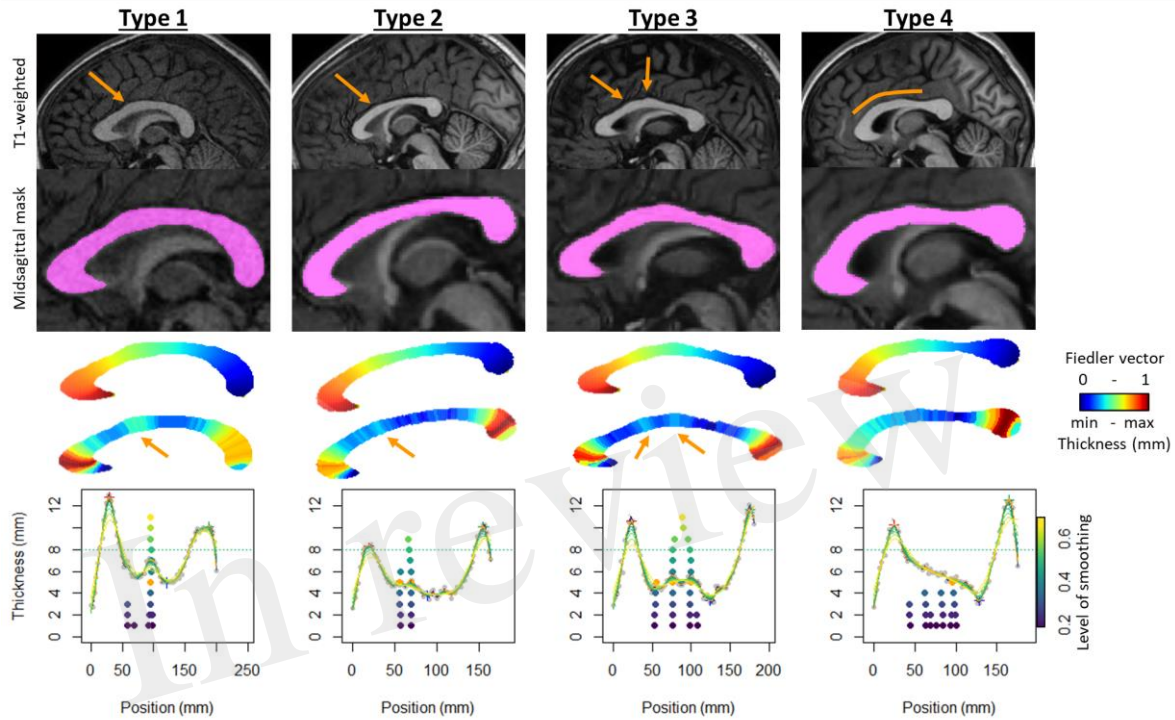
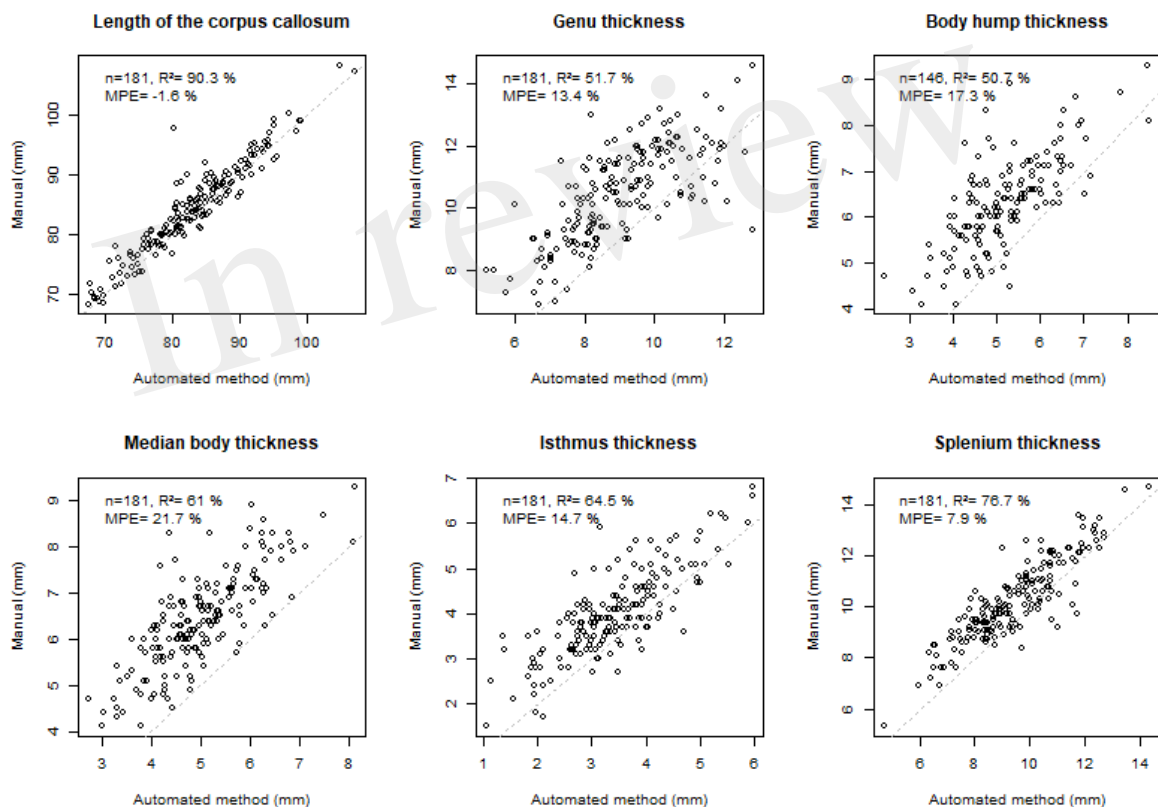


Figure 3. Body hump identification. Example of subject by group, variation of smoothing level to identify local maximums. First row: T1 anatomical image with location of the hump (orange arrow). Second row: the corpus callosum mask on sagittal midsection. Third row: Fiedler vector value (posterior-anterior gradient from 0 to 1). Fourth row: slice thickness (scaled gradient from red greatest to smallest blue thickness). Fifth row: thickness profile as a function of position along the curvilinear abscissa. Variation in smoothing level (colored curves) and position of local maximums between genu and isthmus, from lowest smoothing level (bottom dark purple point) to highest (top light-yellow point). Type 1: position of the body hump obvious and consensual for all smoothing levels. Type 2: position of the body hump obvious and consensual for more than 8 smoothing levels. Type 3: two body humps obvious and consensual for more than 8 smoothing levels. Type 4:

no body hump. **Distribution of types by group: control (C) and FASD (FAS and NS-FASD). Comparison of proportion of type between groups.** ns: f not significant, p-value <0.05; p-values were adjusted for multiple comparisons using the FDR method.

329 The BHT was thus only considered for type 1, 2 and 3 subjects (n=178).

330 The measurements obtained by our method were strongly correlated ($R^2 > 50\%$), with the gold
331 standard of manual measurements, the most highly correlated being that of the LCC ($R^2 = 90.3$
332 %) (**Figure 4**). For this measurement, the error was minimal (mean percentage error
333 MPE=1.6%). This error was moderate for the isthmus, genu and splenium but systematically
334 underestimated (positive MPE < 15%). The manual location for the body thickness
335 measurement (at the central point) did not directly correspond to the measurements
336 collected in the current study, resulting in larger MPE (~ 20%).



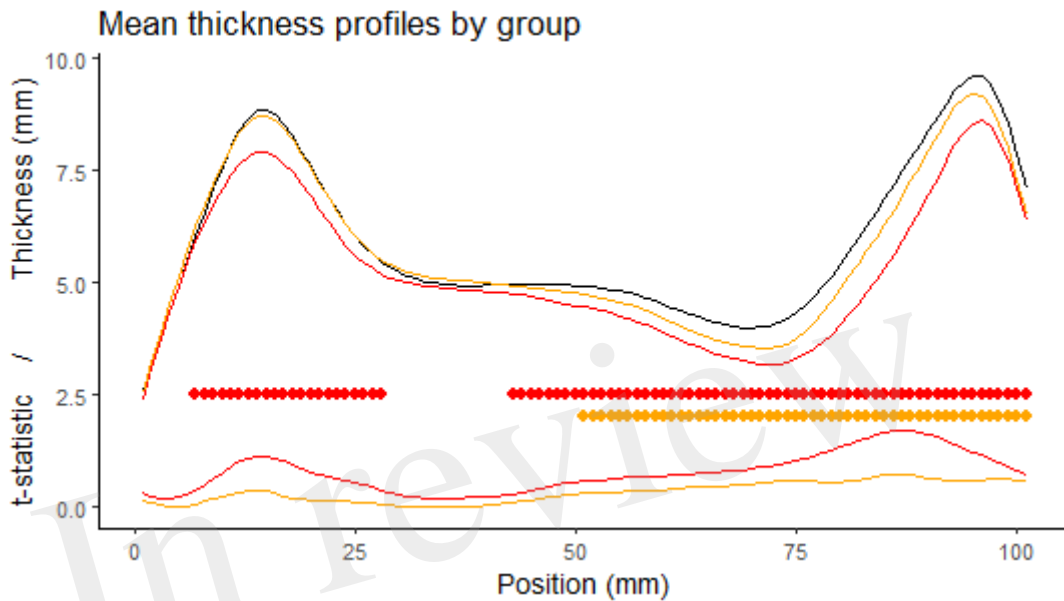
337

338 **Figure 4. Comparison with manual measurements.** Top left: number of subjects (n),
339 coefficient of determination (R^2), mean percentage error (MPE= mean of the difference
340 between manual and automated measurements divided by manual measurement),
341 correlation line 1 to 1 in grey dotted line. Note that, n=181 corresponds to the total number
342 of subjects who had manual measurements in the previous study (Fraize et al., 2023c,
343 excluding the subgroup of 3T controls), n=146 corresponds to the total number of subjects
344 who had manual measurements in the previous study and had hump with type 1, 2, 3.
345 A genetic subjects were excluded.

346 **3.2 Control and FASD comparison**

347 **3.2.1 Unifactorial comparison of thickness profiles**

348 Comparing the thickness profiles of control and FAS subjects after rigid length normalization,
349 we identified two significantly different sections, one around the genu and one consisting of
350 the whole posterior half but with a peak in effect size in the anterior part of the splenium. For
351 NS-FASD, the zone of significance was less extended, and limited to the posterior half (**Figure**
352 **5**).



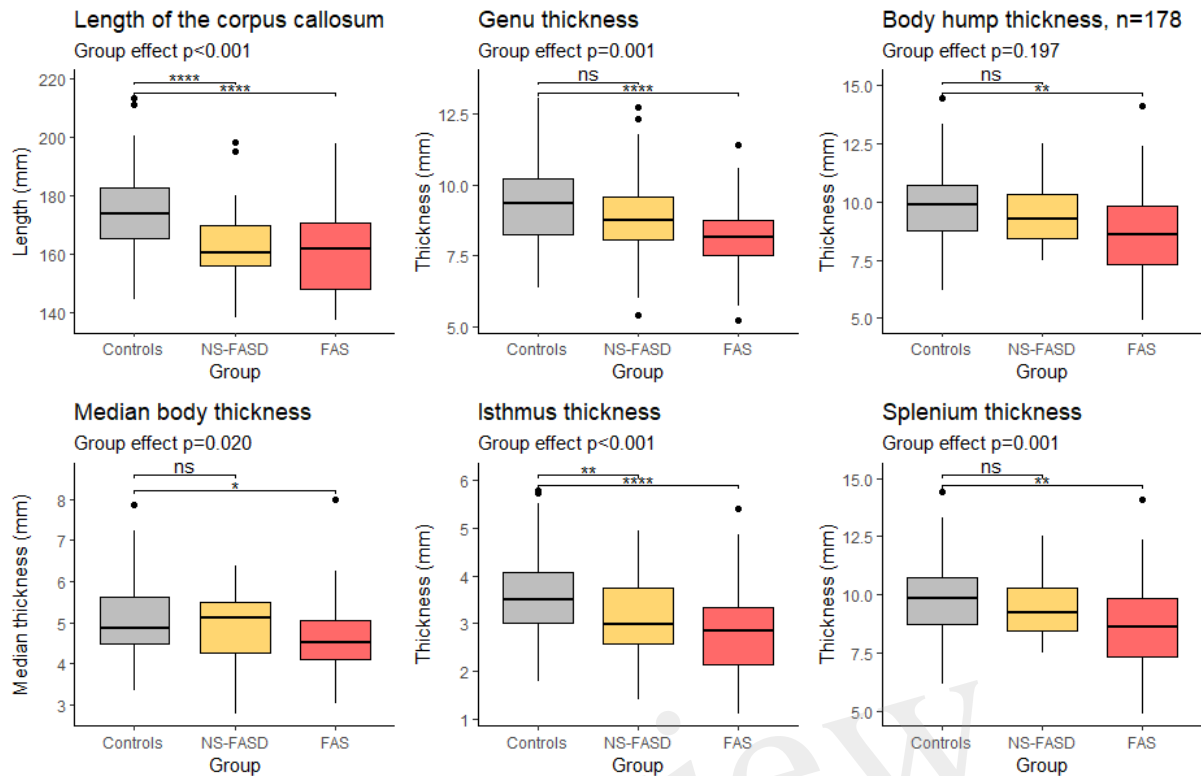
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354 **Figure 5. Comparison of the thickness profiles.** First row: mean profile of the control group in
355 black (n=126), the FAS group in red (n=52), the NS-FASD group in orange (n=37), after rigid
356 length normalization. Second row: cluster of significantly different thicknesses (controls vs.
357 FAS in red or NS-FASD in orange, p-value of cluster mass statistic < 0.05, including adjustment
358 for multiple comparisons). Third row: effect size (t-statistic of the linear mixed model).

359 **3.2.2 Unifactorial comparison of length and thickness of singular points**

360 There was no significantly different proportion of body hump type between the FASD group
361 and the control group. The distribution of types by group is detailed in **Figure 3**.

362 A significant group effect was found for the length of the corpus callosum, the genu, the
363 median body, the isthmus, and the splenium thicknesses. The difference between the control
364 group and the FAS group was significant for all parameters. The difference between the
365 control group and the NS-FASD group was significant only for the length of the corpus callosum
366 and the isthmus thickness ($p < 0.05$) (**Figure 6**).



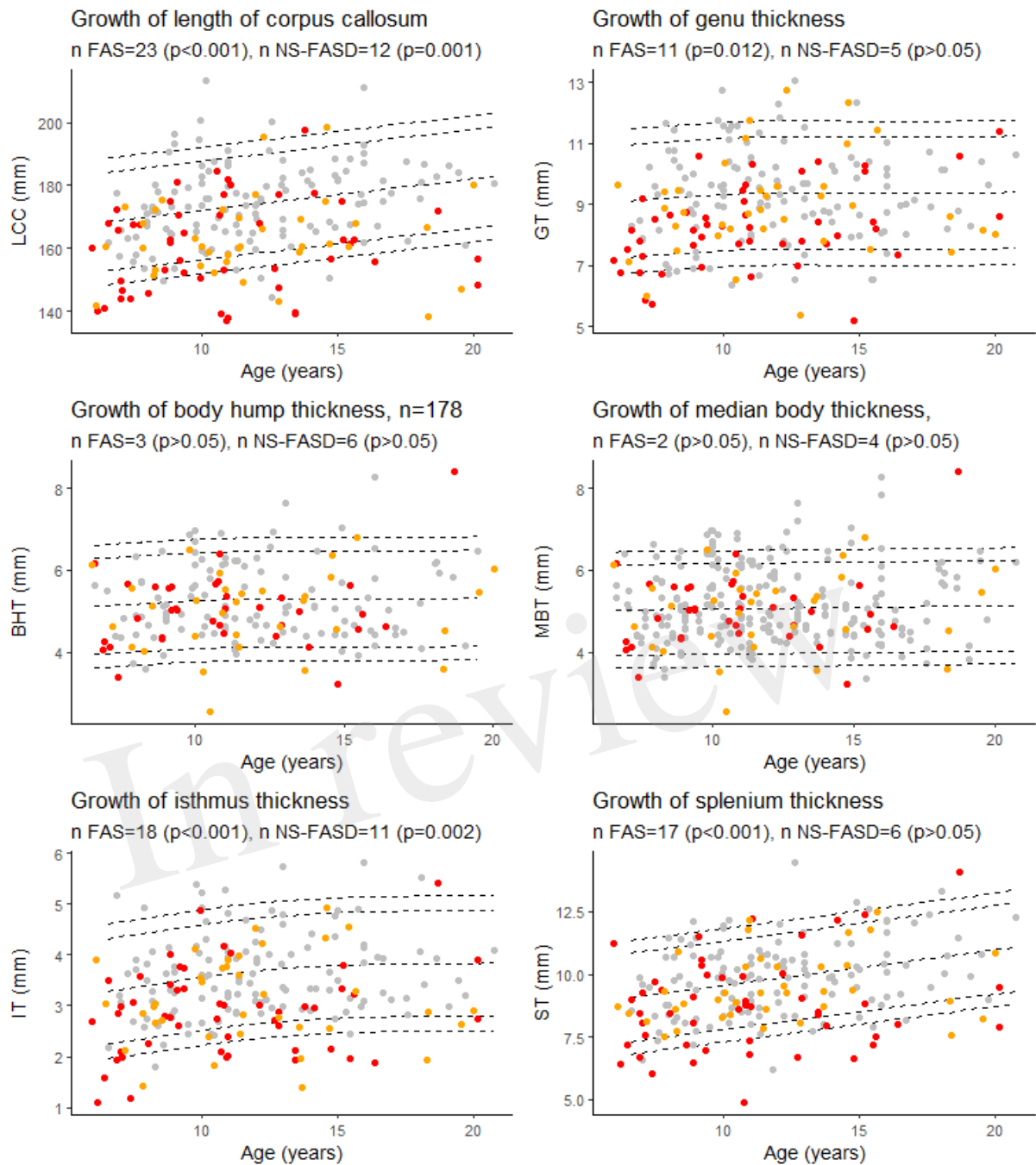
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368 **Figure 6. Comparison of length and thicknesses of singular points.** Group effect (control, FAS
 369 and NS-FASD) on ANOVA. Top bracket, p-value of t-test of controls versus FAS or NS-FASD. ns:
 370 $p > 0.05$, *: $p \leq 0.05$, **: $p \leq 0.01$, ***: $p \leq 0.001$, ****: $p \leq 0.0001$. p-values were adjusted for
 371 multiple comparisons using the FDR method.

372 3.3 Normative analysis

373 3.3.1 Growth charts

374 There was an excess of FASD subjects below the 10th percentile for age for the length of the
 375 corpus callosum, the isthmus, and only for FAS subjects for the genu and the splenium ($p < 0.05$)
 376 (Figure 7).

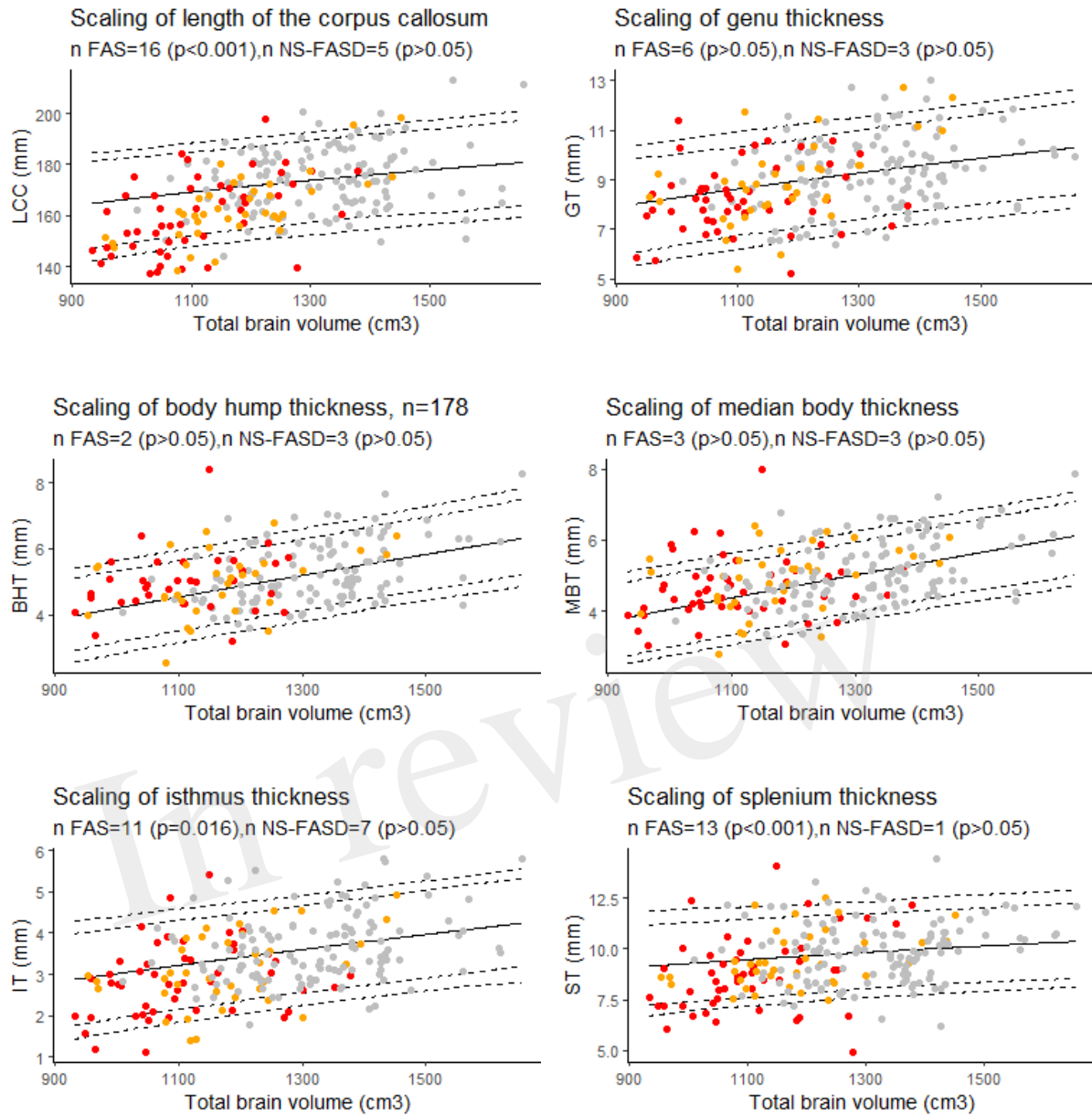


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378 **Figure 7. Growth charts for length of the corpus callosum (LCC), the genu (GT), the isthmus**
 379 **(IT), the body hump (BHT), the median body (MBT), and the splenium (ST) thicknesses.**
 380 Number of fetal alcohol spectrum disorder subjects under the 10th percentile (p-value of
 381 binomial test, p-values were adjusted for multiple comparisons using the FDR method).
 382 Controls in grey, FAS in red, NS-FASD in orange. The 95, 90, 10 and 5th percentiles are
 383 represented in dotted lines.

384 **3.3.2 Scaling charts**

385 There was an excess of FAS subjects below the 10th percentile for brain size for the length of
 386 the corpus callosum, the isthmus, and the splenium (p<0.05). NS-FASD subjects were not over-
 387 represented below the 10th percentile for brain size (p>0.05) (**Figure 8**).



388 **Figure 8. Scaling charts for length of the corpus callosum (LCC), the genu (GT), the isthmus**
 389 **(IT), the body hump (BHT), the median body (MBT), and the splenium (ST) thicknesses.**
 390 Number of fetal alcohol spectrum disorder subjects under the 10th percentile (p-value of
 391 binomial test, p-values were adjusted for multiple comparisons using the FDR method.).
 392 Controls in grey, FAS in red, NS-FASD in orange. The 95, 90, 10 and 5th percentiles are
 393 represented in dotted lines.

395 In this study, we introduce the first fully automated, normalization-free, fast method to
396 produce and analyze the thickness profile of the corpus callosum. We applied it to the
397 morphometric comparison of 89 subjects with FASD to 126 typically developing controls, aged
398 between 6 and 20 years old. We were able to show an apparent downsizing of the corpus
399 callosum both in length and thickness in FAS, predominating in the posterior half and less
400 pronounced in NS-FASD. We established that a recurring abnormal undersizing was observed
401 in FAS only for the length and the isthmic and splenial thicknesses when controlling for brain
402 size. Thus, these results with a new and convenient automated method not only replicate, but
403 also extend our previous results with manual measurements including the same dataset, that
404 were only able to show recurrent isthmic anomaly (Fraize et al., 2023c).

405 4.1 Confirmed and newly revealed differences between FASD and controls

406 4.1.1 What can be observed on native measurements?

407 After rigid linear normalization and adjustment for site, native thickness profiles showed
408 extensive but not homogeneous thinning of the corpus callosum in FASD. It was reduced in
409 the posterior half section in both FAS and non-syndromic FASD subjects and reduced in the
410 genu section only in FAS subjects (**Figure 5**). The rigid anteroposterior deformation
411 coarsely aligns the thickness profiles of each subject, enabling an initial average assessment
412 of what is visible to the radiologist in this population. It points to the posterior zone with a
413 possible additional damage of the genu in FAS and lower severity in NS-FASD.

414 Considering the native thickness of the four singular local extrema (genu, body hump, isthmus,
415 and splenium), we observed significant differences between the FAS and the control groups
416 for all these extrema and between the NS-FASD and the control groups for the isthmus only
417 (**Figure 6**). However, the effect on body thickness appeared much smaller, and was not
418 significant when the 3 groups were compared together (ANOVA). In addition, we showed no
419 impact of FASD on body hump morphology, since there was no significant difference in the
420 proportion of body hump type between groups ($p < 0.05$) (**Figure 3**). A recent study has evoked
421 and dismissed the over-representation of “notching” among subjects with FASD (Schneble et
422 al., 2020), in the medico-judicial context of FASD recognition, but using a very qualitative
423 assessment. Our results are consistent with the fact that the body and its possible hump(s)
424 are spared from callosal thinning in FASD, which may be seen as clinically relevant *per se*.

425 We also showed that the overall length of the corpus callosum was reduced ($p < 0.001$) on
426 average, with no other adjustment than site effect, in both NS-FASD and FAS (**Figure 6**). All
427 these results are consistent with previous studies describing a smaller corpus callosum (Riley
428 et al., 1995; Sowell et al., 2001; Astley et al., 2009; Biffen et al., 2017; Jacobson et al., 2017;
429 Fraize et al., 2023c) and pointing out the posterior part as the most affected one (Sowell et
430 al., 2001; Yang et al., 2012a; Fraize et al., 2023a). Yet, even if our FASD and control groups
431 were matched for age and sex, there were inherent differences in brain size, both age and size
432 having potentially nonlinear effects to be accounted for in further analyses.

433 4.1.2 What remains at the individual level after independent control of major covariates?

434 Since birth, the shape of the corpus callosum changes as revealed by morphometric
435 parameters (Rajapakse et al., 1996; Westerhausen et al., 2011; Herron et al., 2012). Within
436 the increasingly promoted and clinically relevant framework of normative analyses, we
437 proposed to take age into account on the basis of developmental growth charts derived from
438 our typically developing control sample. We found FAS-recurrent anomalies (excess of FAS
439 subjects below the 10th percentile) for the LCC, the genu, the isthmus, and the splenium
440 thicknesses (**Figure 7**). This means that considering the age effect did not modify our previous
441 description of the large downsizing of the corpus callosum both in length and thickness in FAS,
442 predominating in the posterior half and in the genu. This minor effect of age on the
443 measurements is consistent with asymptotic linear low (length, splenium) or null (other
444 thicknesses) residual growth of the corpus callosum after 6 years already described in the
445 typically developing pediatric population (Garel et al., 2011; Fraize et al., 2023c).

446 In the FASD population with brain growth deficiency (Archibald et al., 2001; Astley et al., 2009;
447 Rajaprakash et al., 2014; Treit et al., 2016; Boronat et al., 2017), brain size must be properly
448 considered when interpreting other neuroanatomical measurements. Thus, to describe the
449 reduction of the corpus callosum measurements observed in FASD at the individual level, we
450 added to the classical normative analysis on growth charts (effect of age) the analysis on
451 scaling charts (effect of size). We ensured that the scaling model fitted in the control group
452 correctly projected to the smaller FASD range of brain sizes by using a biomathematical model
453 that captures the gradual change in proportions along size range. This allometric scaling was
454 modelled by a power law whose relevance and interest have been widely argued and
455 documented (Germanaud et al., 2014; Liu et al., 2014; de Jong et al., 2017; Warling et al.,
456 2021). It is already used in anatomical descriptions of the corpus callosum in newborns (Lewis
457 et al., 2022). Hence, using allometry-sensitive scaling charts to account for brain size effect,
458 we showed that thinning (below the 10th percentile) remained recurrently abnormal in FAS
459 only for the isthmus and the splenium thickness (**Figure 8**). We additionally showed a
460 significant excess of FAS subjects with undersized total LCC for their brain size (**Figure 8**). So,
461 we confirmed and extended the results of our previous study (Fraize et al., 2023c), by adding
462 both brain size independent antero-posterior length and splenium thickness impairments to
463 that of the isthmus. This involvement of the splenium is also consistent with our previous
464 findings showing a reduction of its posterior half surface independent from hemispheric size
465 (cortical surface) in a subsample of subjects (Fraize et al., 2023a).

466 These new findings may be explained by the greater number of controls (n=126 vs. 94), the
467 more reliable estimate of brain size (total brain volume vs. surface of a reference brain area),
468 the more elaborate model of regression and the more robust assessment of percentiles (Fraize
469 et al., 2023c). The addition of the ComBat batch effect adjustment could also have improved
470 sensitivity (see **Table 2, sup. mat.**). Previously, there was no significant site effect to be
471 corrected in the manual measures (Fraize et al., 2023c). In this case, *post hoc* analyses without
472 adjustment for batch effect showed no difference in the present results (data not shown). It
473 is also possible and a reasonable assumption that automated measurement of thickness of
474 the splenium is more accurate and less noisy, enabling more discriminating statistical
475 comparison.

476 *4.1.3 Potential neuroanatomical markers of FASD in corpus callosum*

477 We did not find any size-independent recurrent anomalies taken one by one in our small NS-
478 FASD subgroup. But for these subjects we have already proposed a perspective of cumulative
479 diagnostic probability for diagnostic improvement (Fraize et al., 2023c). Arguably, the
480 likelihood of the causal link with alcohol exposure increases for NS-FASD subjects with one or
481 more anomalies found to be recurrent in FAS in the final scaling analysis (LCC, IT, ST, in **Figure**
482 **8**). In this case, these new results in FAS could provide additional diagnostic arguments and
483 ease the way to more confident diagnoses in certain subjects presenting FASD without FAS.

484 Yet, the posterior damage of the corpus callosum with preservation of the body is probably
485 not specific to FASD, as callosal anomalies are not rare in the general (Glass et al., 2008) nor
486 in the neurodevelopmentally disabled population (Jeret et al., 1985). But we have already
487 argued that the entire corpus callosum morphology could constitute a radiological signature
488 likely to increase diagnostic certainty, particularly in NS-FASD. Moreover, other focal
489 neuroanatomical anomalies such as cerebellar damage (O'Hare et al., 2005; Cardenas et al.,
490 2014; Sullivan et al., 2020; Fraize et al., 2023b) or deep grey nuclei volume reduction (Nardelli
491 et al., 2011; Roussotte et al., 2012; Nakhid et al., 2022), should also be considered in a
492 composite, multidimensional neuroanatomical score reflecting fetal alcohol-induced brain
493 dysmorphia.

494 4.2 New method for analyzing the shape of the corpus callosum

495 Our new method for corpus callosum shape analysis was developed to automatically detect
496 the anterior point of the rostrum and decide on a posterior point of the splenium. It is
497 advantageous over the existing ones because it does not require human intervention (Luders
498 et al., 2006b; Adamson et al., 2011) and does not involve spatial normalization (Herron et al.,
499 2012). In its current state, only the existence of a rostrum is considered. Our method is based
500 on the maximum elongation of this two-dimensional shape, so it can accommodate any
501 posterior shape of the corpus callosum. The three cases of agenesis or incomplete corpus
502 callosum prove that this method is robust to variation of corpus callosum shape, even
503 pathological (**Figure 2**), at least posterior ones. In these agenetic cases, we did not integrate
504 the detection of singular points, which are not consensual and would require human
505 supervision. For all subjects, this method produced continuous thicknesses along the entire
506 length of the corpus callosum, and unequivocally detected singular local extrema at singular
507 points (the genu, the hump of the body, the isthmus, and the splenium). Extracted thickness
508 measurements were highly correlated with the gold standard manual measurements (**Figure**
509 **4**), despite a small to moderate underestimation ($MPE < +15\%$). The two methods deal with
510 partial volume effects on the edges differently. The manual process relies on the visualization
511 smoothing included in the PACS viewer that could potentially biased the eye of the expert.
512 The automated one relies on the segmentation of the mask of the corpus callosum – based on
513 the contrast between grey matter, white matter and CSF – providing a skinnier or even eroded
514 profile, logically resulting in a higher MPE for small measures than for large ones (genu, body,
515 isthmus). Bear in mind that noise could also be induced by inaccuracy of the thinnest
516 measurements close to the resolution of the oversampled mask (0.5 x 0.5mm). Finally, even if
517 manual measurement is the gold standard, the automated method may be more objective,
518 reproducible, and less sensitive to global brain shape variation.

519 The first step, i.e., producing the mask of the corpus callosum on the sagittal section, may
520 seem trivial but is in fact a decisive one. In our pipeline, this step was based on robust

521 intensity-based *Morphologist* segmentation bricks, but a quality check was systematically
522 performed, and manual corrections were sometimes necessary. Our method could benefit
523 from the use of other software able to provide the 2D voxel-based mask, for example
524 *Freesurfer* (actually 3D) or any new and specific methods (Adamson et al., 2014; Herrera et al.,
525 2022), without modifying the subsequent steps. Ultimately, although not all steps are
526 encapsulated and seamlessly connected, our new tool offers the advantage of having
527 extremely short and computationally inexpensive steps. As a result, the cumulative
528 computation time per subject to generate numerical parameters is less than 5 minutes.

529 On a methodological aspect, the correction of the Fiedler vector to reposition the rostrum is
530 an example of partially-supervised information (a priori-based) in an otherwise unsupervised
531 context (Lefevre et al., 2023). It may be possible in the future to add other kinds of
532 information, of various kinds (lines), to add constraints on the Fiedler vector or more generally
533 on the Laplacian modes. More broadly, the developed methodological tool based on the
534 Fiedler vector opens the way to other fields of characterization of the shape of the corpus
535 callosum, such as the circularity, the surface per slice, or deformation per section, which could
536 be the object of further study (Coulon et al., 2015; Walsh et al., 2019).

537 For now, as far as we know, this is the only fully automated method without any human
538 intervention and normalization step for obtaining corpus callosum thicknesses. In fact, its use
539 could go far beyond FASD and be applied in other pathologies where the morphology of the
540 corpus callosum needs to be described.

541 4.3 Translating to daily clinical practice

542 In this study, we aimed to establish an analysis protocol that would ultimately be compatible
543 with translation to clinical practice. The ultimate goal is to switch from manual measurements,
544 which may be imprecise and noisy if non-expert, to secure computational automated and fast
545 measurements, which could be facilitated by a computer interface. The proposed tool and
546 analysis protocol should be acceptable in clinical practice because the produced
547 measurements correspond to those already made in clinical settings (Garel et al., 2011;
548 Ambrosino et al., 2022; Fraize et al., 2023c), and because their anatomical positioning is
549 probably more objective. Acceptability should also be promoted by the fact that it leads to a
550 normative analysis and therefore to categorial (normal, abnormal) information at the
551 individual level.

552 Based on easy-to-use scaling charts and a proper biomathematical scaling model, we propose
553 a method for detecting subject-level abnormalities, even with the partial overlap of brain size
554 between patients and controls. However, the choice of reference population and adequacy of
555 the control group raise questions. Our study included 126 typically developing individuals
556 matched for age and sex, with no prenatal exposure. The automated segmentation, profiling,
557 and singular local extrema detection enable the use of large imaging databases to establish
558 more reliable charts, potentially stratified by age and sex. Despite the need to address site
559 effects, our results show that a population of over a hundred controls currently allows for the
560 establishment of informative normative charts.

561 4.4 Identification of a singular thickening of the body section in the general population

562 Our method leads to the description of a possible anatomical particularity of the corpus
563 callosum, in FASD and more generally in healthy subjects. We identified a local thickening of
564 the body section, either single (~70%) or double (16%) in most of the subjects (**Figure 4**). This
565 local maximum of the thickness profile between the genu and the isthmus was automatically
566 identified by using multi-scale-smoothed profiles inspired by scaled space implementation
567 detecting robust maxima through a range of smoothing levels. This is almost equivalent to
568 applying an amplitude limit without having to quantify the hump in mm in subjects with
569 varying CC sizes. The literature on this morphological feature in the general population is
570 sparse (Krause et al., 2019; Simpson et al., 2020). Krause et al., reviewed MR images of the
571 corpus callosum of over 1,600 healthy subjects and denominated concavities in the dorsal
572 surface "undulations" and "notching". They found 50% of subjects with one notch and around
573 10% with two, and therefore possibly equivalent proportions of localized thickening.

574 We decided to add the median of the body thickness for all subjects, to compensate for the
575 lack of consensus on the actual existence of this hump and the absence of an exact definition
576 for the location of the body thickness measurement (Garel et al., 2011). This corresponds to
577 the median value of the thicknesses on the section between the genu and the isthmus.
578 Although it was somewhat arbitrary, it correlated well with the manual measurement ($R^2 =$
579 61%). In practice, and even if this is a finalist argument, the results were ultimately consistent
580 between the two measures.

581 **4.5 Other limitations and future directions**

582 One limitation of the proposed modeling for analyses is the lack of consideration for the effect
583 of sex (Ardekani et al., 2013; Lewis et al., 2022). We made this choice on the hypothesis that
584 the downsizing of the control sample by a factor of two to establish sex specific charts would
585 have lowered the statistical power of our study too much. We would have increased the risk
586 of missing results, even with a reduced residual variance due to better adequacy of the
587 modeling. It is a questionable choice that we also made and argued for our previous study,
588 showing that results were almost unaffected (meaning that with this population size, the two
589 choices may probably be equivalent). Yet as mentioned previously, with larger databases
590 being available, it will be more efficient, even with clinical applications in mind, to establish
591 differentiated female/male referential charts. It could also very well lead to the description of
592 differential FAS-related abnormalities and markers between males and females (Chen et al.,
593 2011; Zhou et al., 2018; Little and Beaulieu, 2020; Treit et al., 2020).

594 The limitations associated to our cohort of FASD subjects are multiple: retrospective data,
595 absence of quantitative data on the level of exposure, over-representation of FAS subjects.
596 But we would like to confirm, since this is not possible or recommended in all countries, that
597 in our practice, brain imaging is systematic. There is no predictable bias in severity or clinical
598 representation related to MRI availability.

599 **5 Conclusion**

600 Our study is the first to propose a fully automated tool to assess the corpus callosum thickness
601 profile along its curvilinear abscissa and analyze it through the identification of 4 singular
602 points. We used it to describe the callosal damage in a large cohort of FASD. We confirmed
603 the excessive thinning of the isthmus for brain size. We revealed the global excessive
604 shortening of the corpus callosum and thinning of the splenium for brain size to be recurrent

605 anomalies in FAS subjects. The introduction of this tool in clinical practice is at hand and our
606 study completes the knowledge on FASD callosal damage and reinforces the conviction that a
607 neuroanatomical signature of FAS could be searched for in NS-FASD to improve the specificity
608 of the diagnosis.

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615 Conflict of interest statement

616 The authors have no conflicts of interest to disclose.

617 Data availability statement

618 The data that support the findings of this study are available on request from the
619 corresponding author. The data are not publicly available due to privacy or ethical restrictions.

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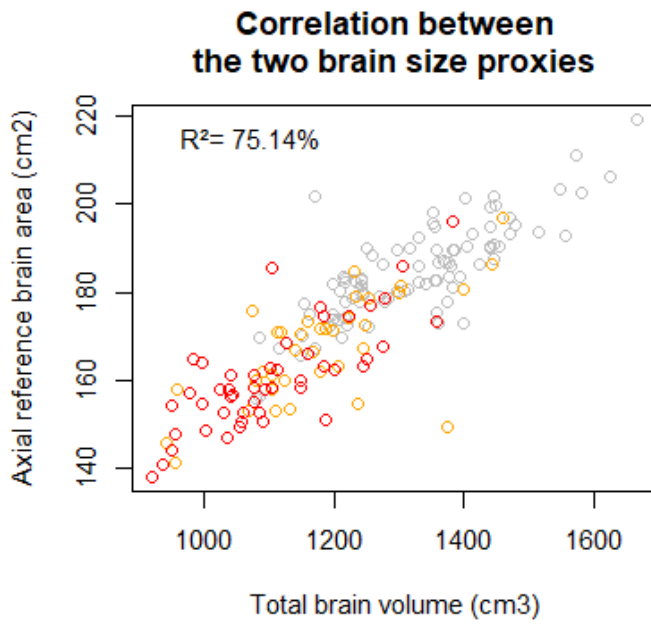
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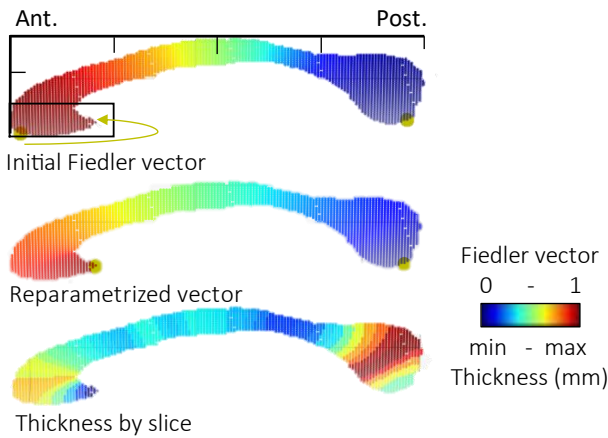


881

882 **Figure 1.** Correlation between the two proxies of brain size, the total brain volume from
883 Volbrain and the axial reference brain area (measurement previously described in Fraize et al.,
884 2023c. Top left, R² coefficient of correlation. Controls in grey, FAS in red, NS-FASD in orange.

Algorithm for repositioning the rostrum in optimal position

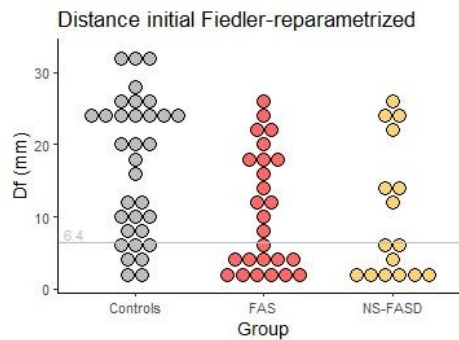
(posterior point of the lower third of the first quarter; in reference where the maximum elongation was observed)



Quantification of the distance between initial rostrum position and the reparametrized extremity (D_f , mm) and comparison by group.

	Well positioned $D_f=0$	Short repositioning $D_f < 6.4$	Large repositioning $D_f > 6.4$
Total (n=213)	138 (64.8%)	26 (12.2%)	49 (23.0%)
Controls (n=126)	93 (73.8%)	7 (5.6%)	26 (20.6%)
FASD (n=87)	45 (51.7%)	19 (21.8%)	23 (26.4%)
Comparison %control vs. FASD	p=0.002	p=0.001	p=0.410

D_f of control and FASD,
Control in grey
FASD in red
Threshold 6.4 in dotted line



885

886 Figure 2. Algorithm for repositioning the rostrum in optimal position.

887 **Table 1. Manual correction of the mask of the corpus callosum by group.**

	FAS	NS-FASD	Controls
	n = 52	n = 37	n = 126
Manually corrected	30.8%	32.4%	62.7%

888

889 **Table 2. Effect of scanner, age, and sex on raw measured parameters in the control group.**

	Age effect	Sex effect	Scanner effect
	p ^a	p ^a	p ^a
Length of the corpus callosum	0.009	0.043	0.033
Genu thickness	0.659	0.186	0.022
Body hump thickness	0.659	0.015	0.021
Body median thickness	0.659	0.010	0.002
Isthmus thickness	0.058	0.001	0.001
Splenium thickness	0.001	0.036	0.450

890 Multivariate linear regression.

891 Bold type, p<0.05, after FDR correction.

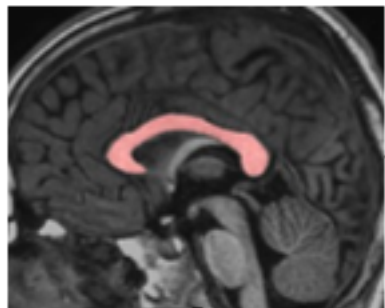
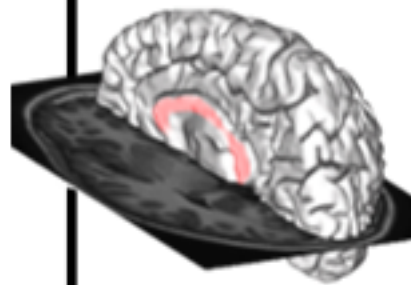
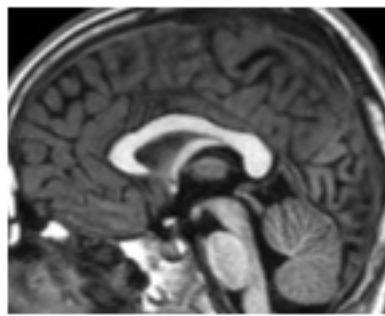
892 ^a p-value from the generalized linear model including scanner, age, and sex as covariates for
893 each parameter measured.

894 **Table 3. Percentage change due to site effects correction per Combat.**

	Correction (%)
Length of the corpus callosum	-0.09
Genu thickness	0.31
Body hump thickness	-3.06
Body median thickness	0.45
Isthmus thickness	0.71
Splenium thickness	0.07

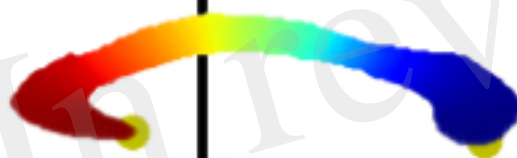
895 Correction = mean of (corrected value - native value)/ native value, expressed as a percentage

Production of midsagittal mask of the corpus callosum

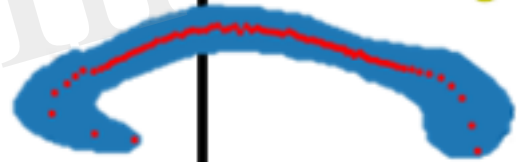


Quality check and manual correction if needed

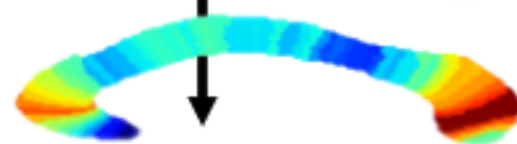
Spectral analysis of the shape using Fielder vector



Identification of the two extremities of the elongated shape

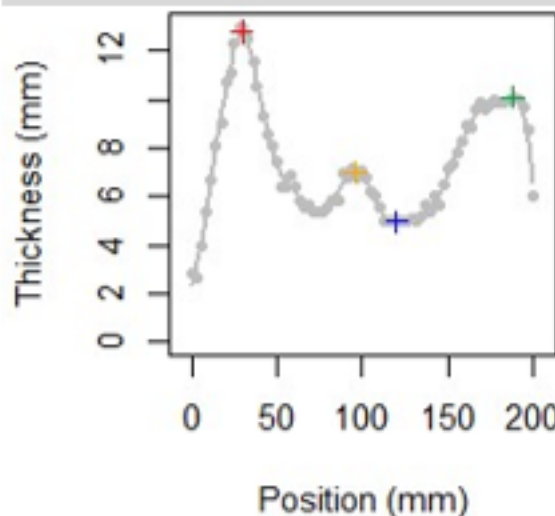


*Delineation of midline
Extraction of LCC*



Measurement of thickness slice by slice

Detection of singular points on thickness profile



*Genu: anterior max.
Body: local max.*
Isthmus: posterior min.
Splenium: posterior max.
Position and thickness for each points*

Figure 2.TIF

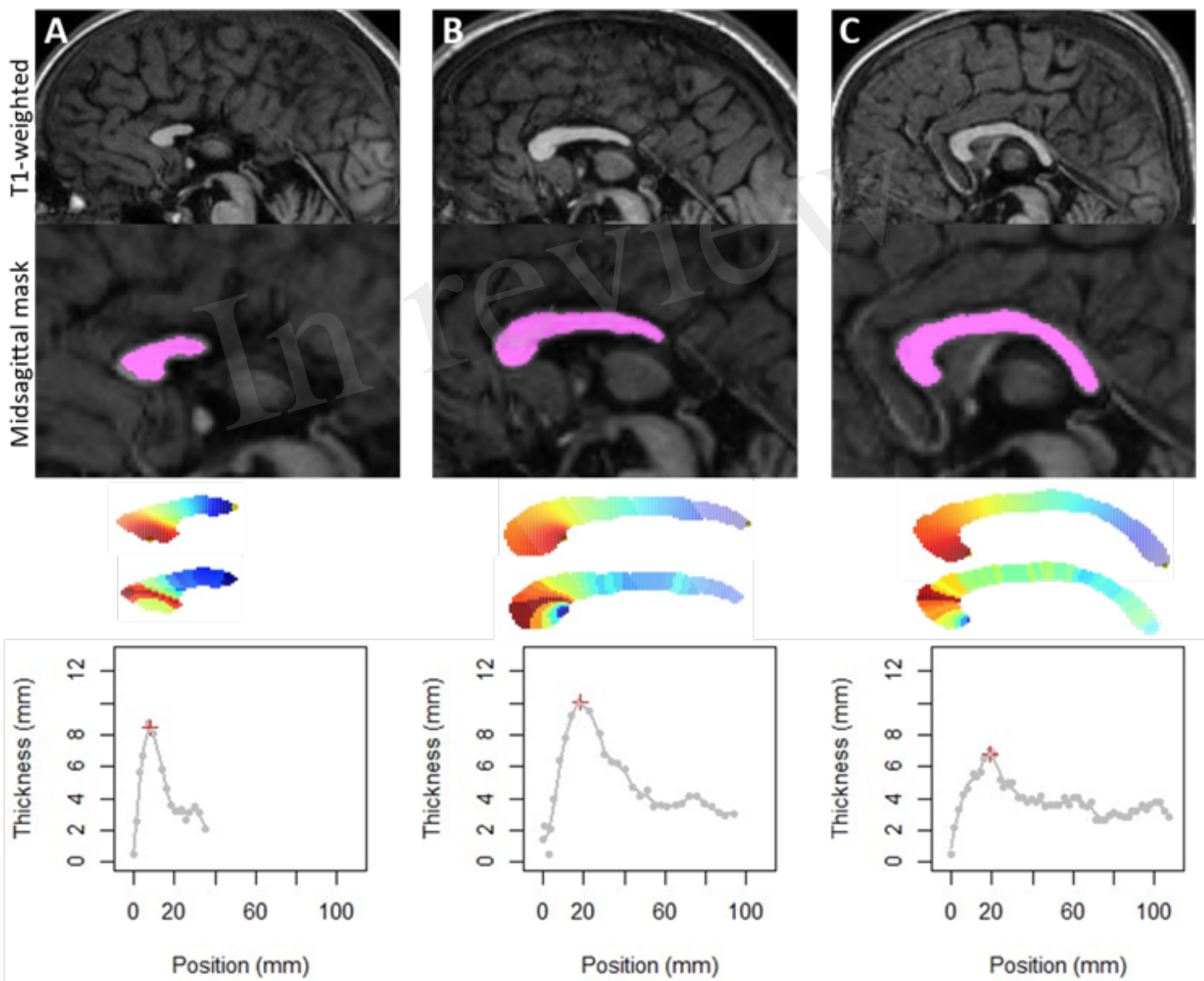


Figure 3.TIF

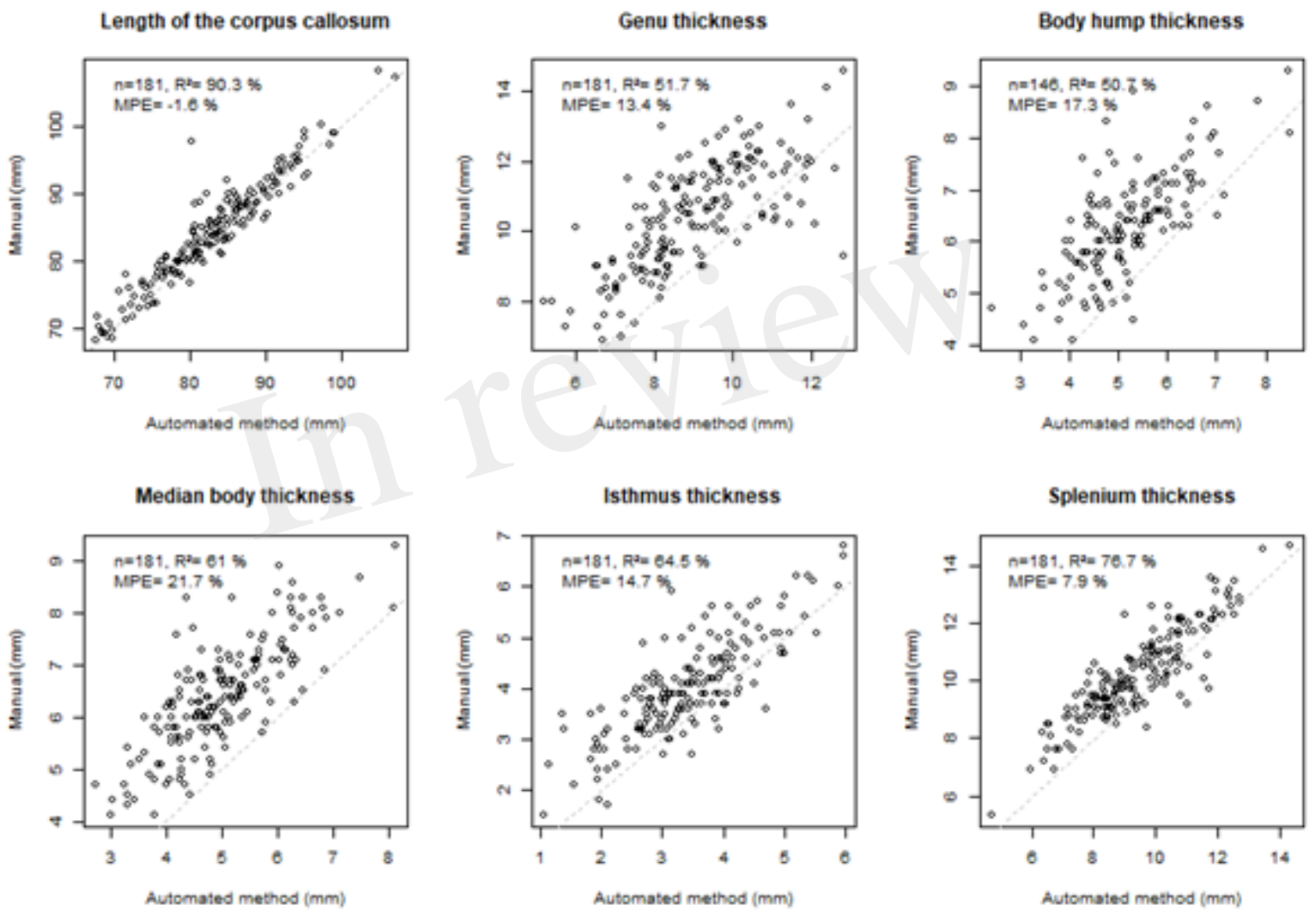


Figure 4.TIF

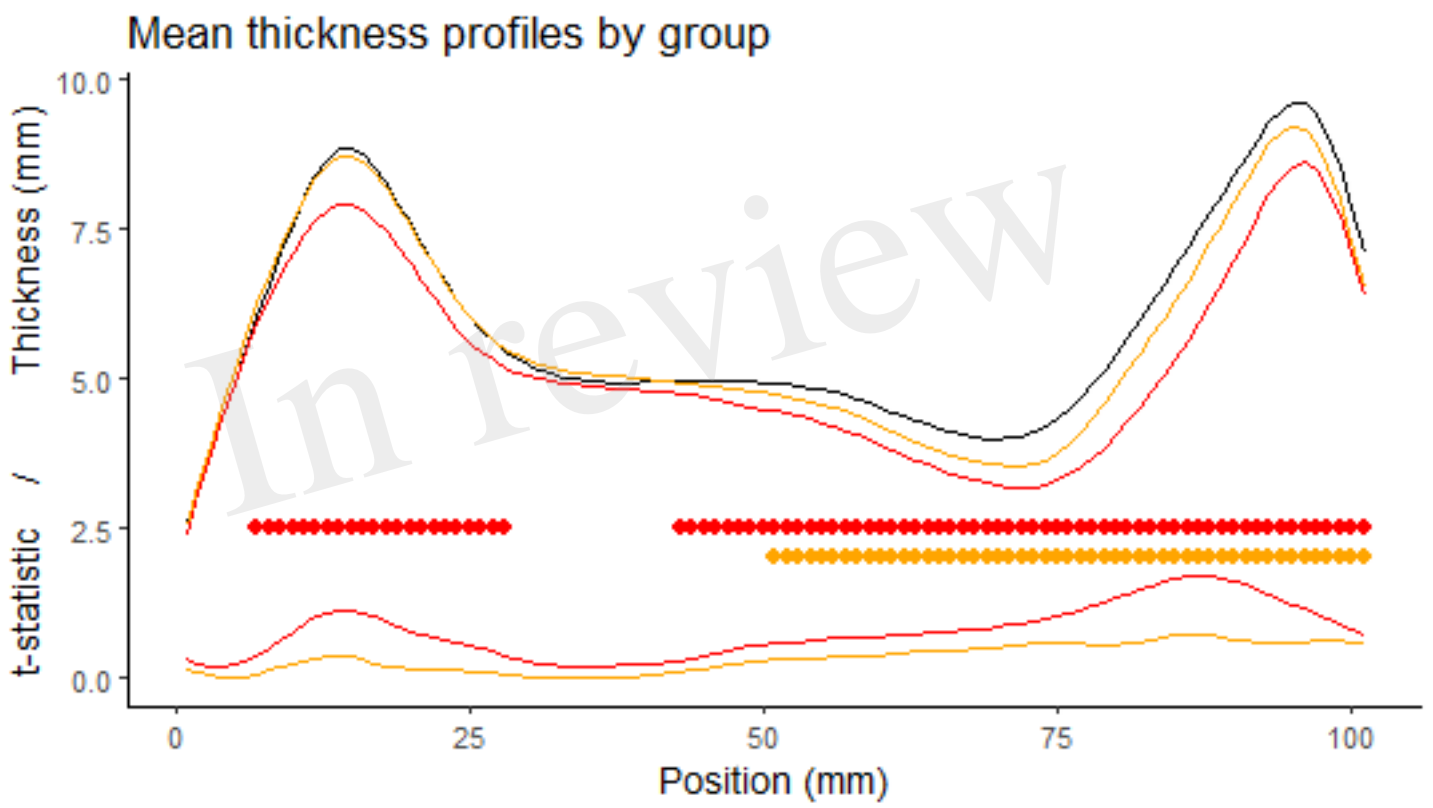


Figure 5.TIF

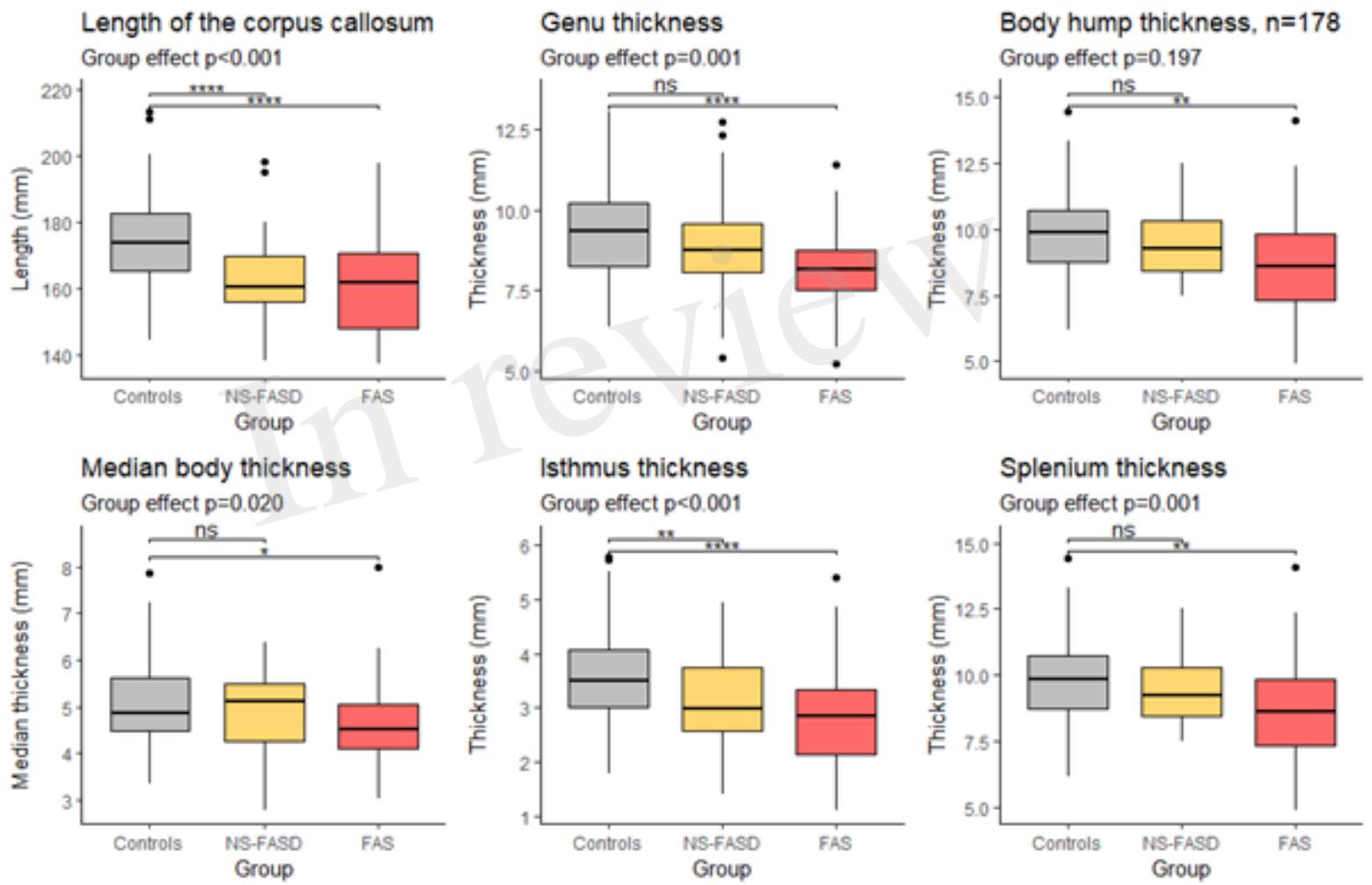


Figure 6.TIF

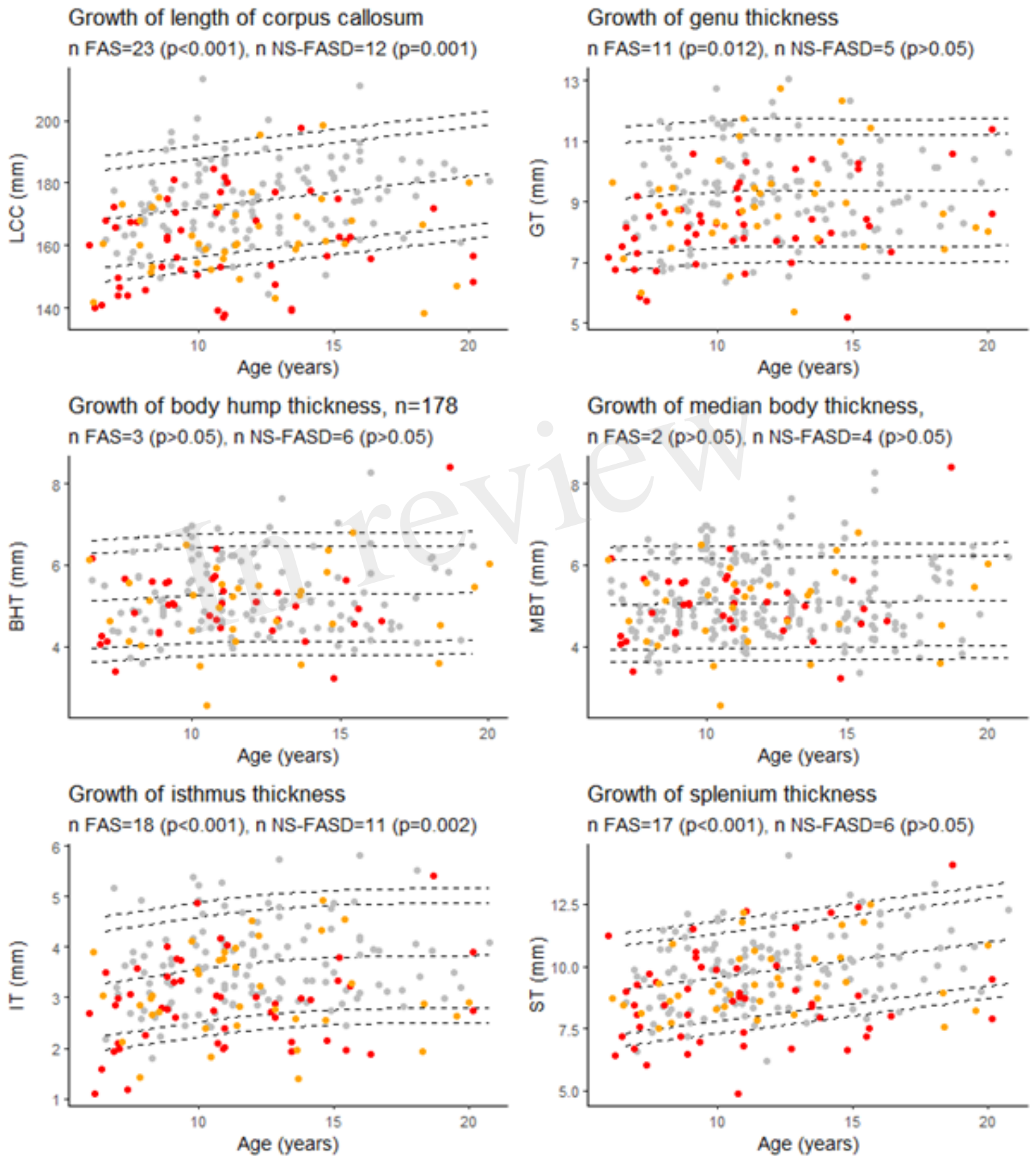


Figure 7.TIF

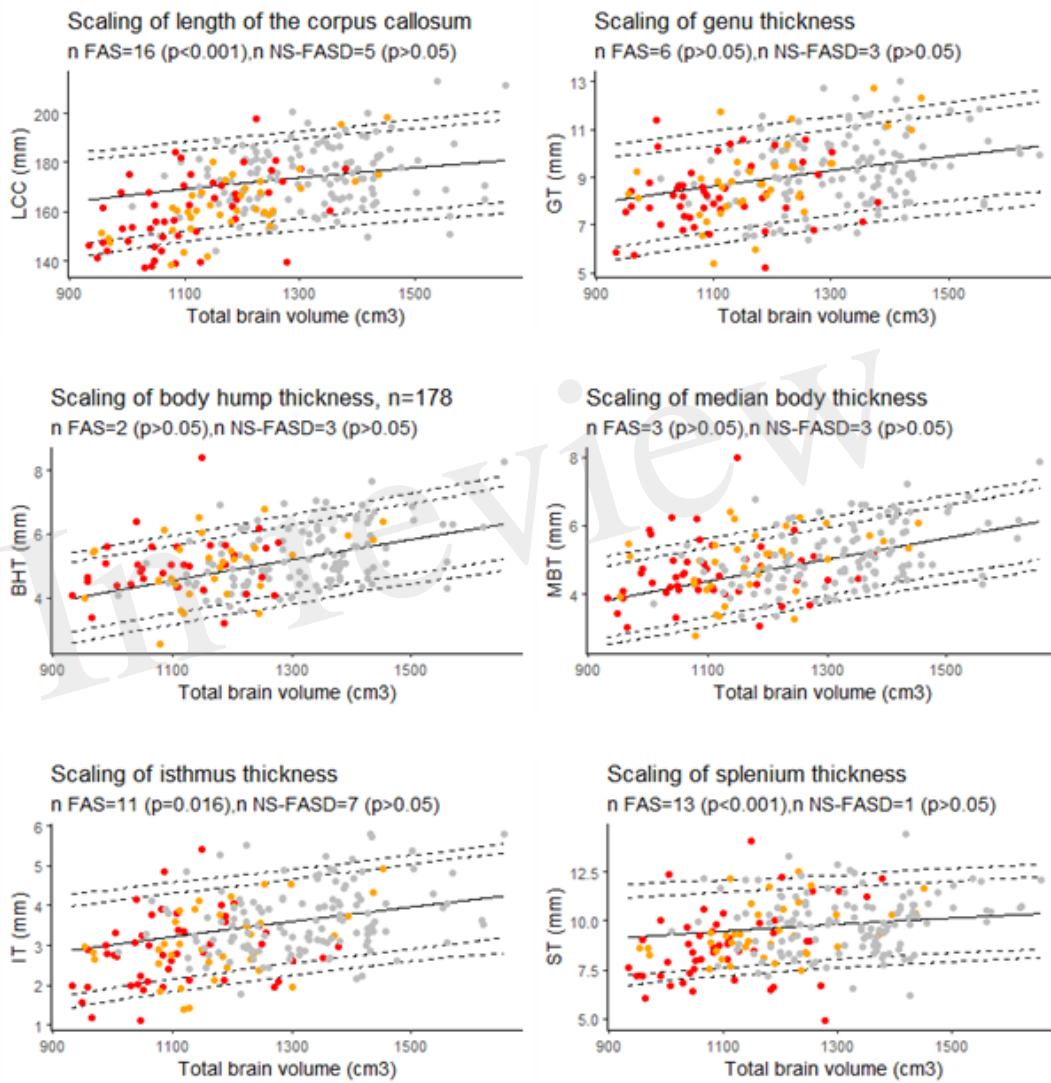
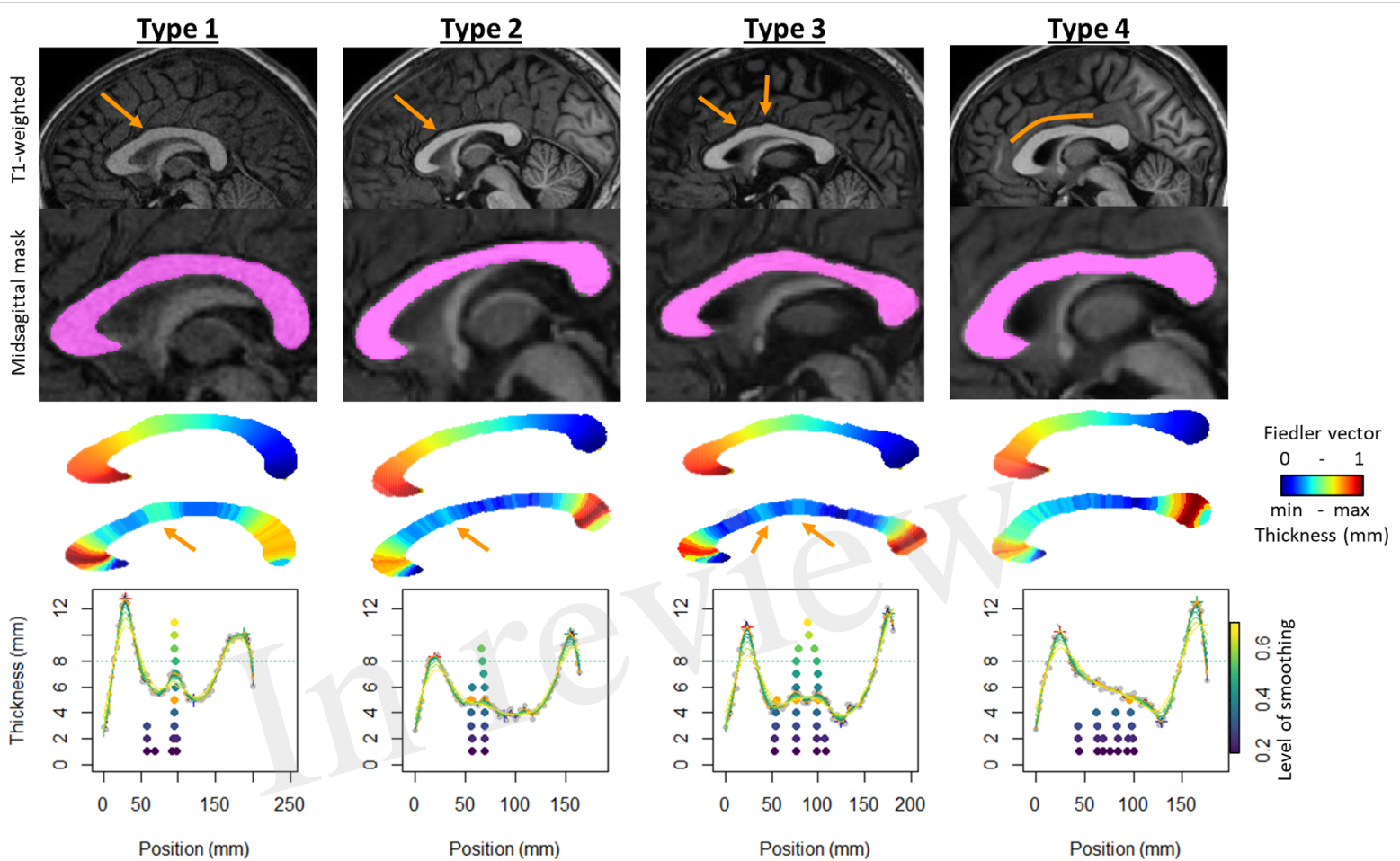


Figure 8.TIF



Type of body hump

